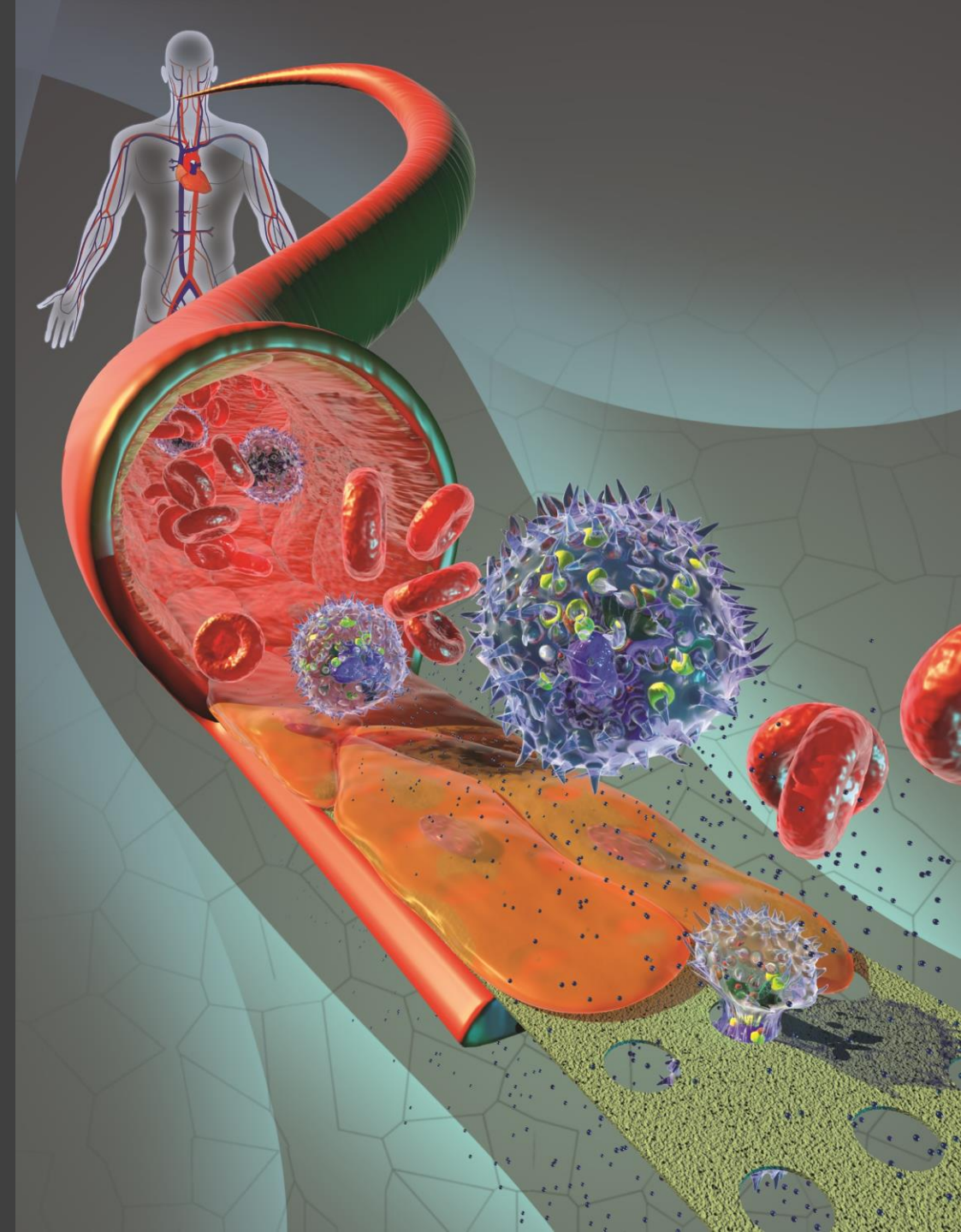


Pulmonary Microvasculature Mimetics for Investigating the Role of Endothelial Apicobasal Polarity in Inflammation and Sepsis

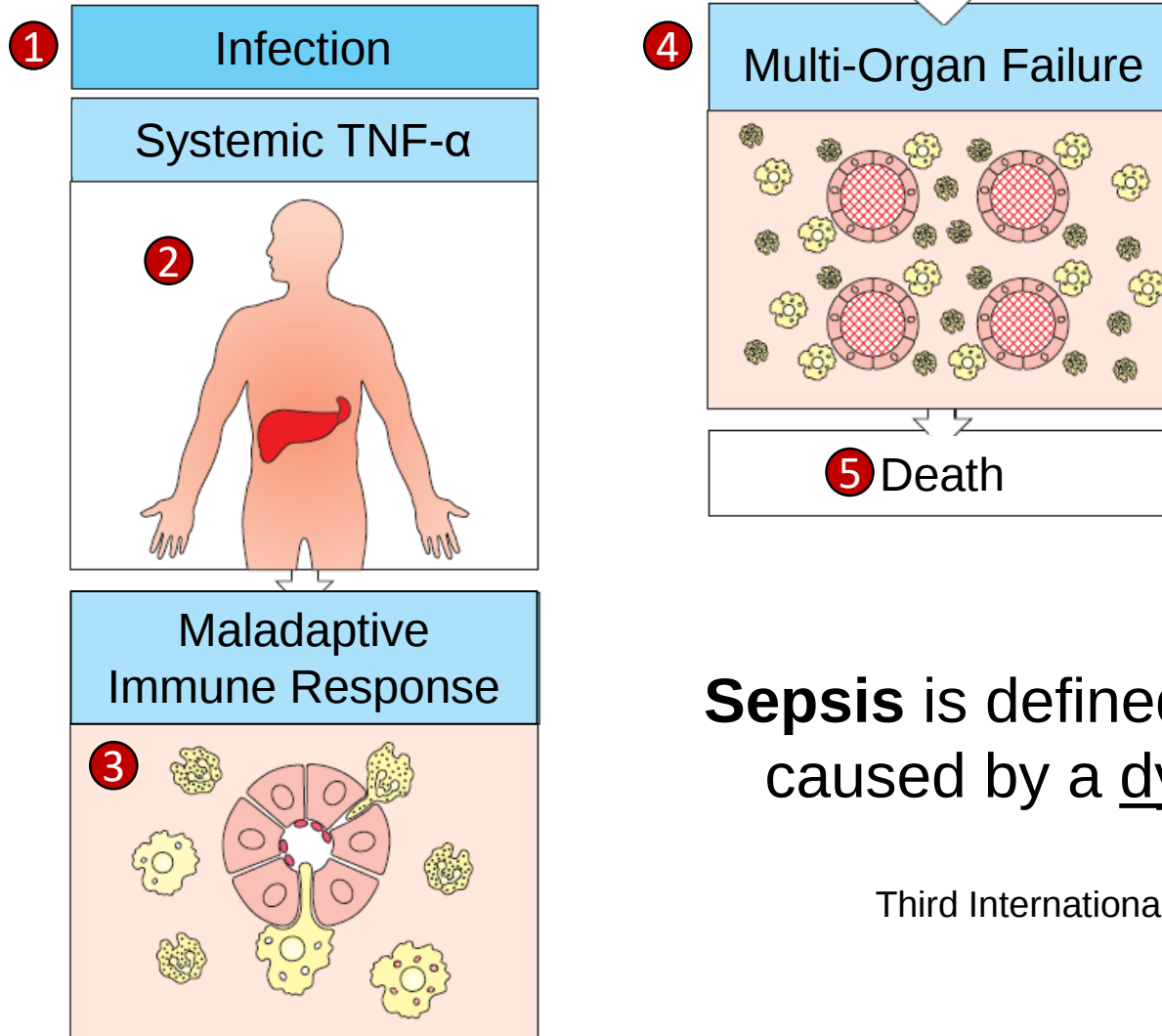
Proposal Presentation

Alec Salminen

April 16th, 2019



Pathophysiology of Sepsis



Sepsis is defined as a life-threatening organ dysfunction caused by a dysregulated host response to infection

Third International Consensus Definitions for Sepsis and Septic Shock **2016**

Sepsis in The Clinic



Global sepsis cases total ~31.5 million each year, with ~5.3 million resulting in death (**15-25% mortality**)



In the USA, this amounts to ~**250,000 deaths** annually



Clinical treatment mainly consists of managing symptoms (fluid replacement, ventilation) and antibiotics



Defining Sepsis in The Clinic: SOFA Score

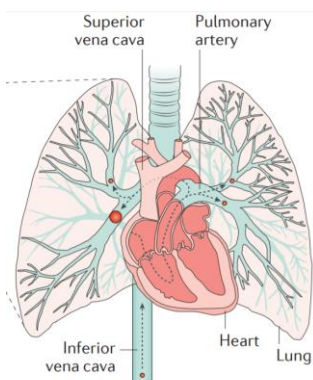
The **sequential organ failure (SOFA) score** is utilized in the clinic to predict and track patient outcome due to complications of sepsis

TABLE 1. SEQUENTIAL ORGAN FAILURE SCORE

	0	1	2	3	4
Ventilation: PaO ₂ :FiO ₂ , mm Hg	>400	≤400	≤300	≤200 ^a	≤100 ^a
Coagulation: platelets × 10 ³ /mm ³	>150	≤150	≤100	≤ 50	≤ 20
Liver: bilirubin, mg/dL (micro- mol/L)	<1.2 (<20)	1.2–1.9 (20–32)	2.0–5.9 (33–101)	6.0–11.9 (102–204)	>12.0 (>204)
Cardiovascular	No hypotension	Mean arterial pressure <70 mm Hg	Dopamine ≤5 or dobutamine (any dose) ^b	Dopamine >5 or epinephrine ≤0.1 or norepinephrine <0.1 ^b	Dopamine >15 or epinephrine >0.1 or norepinephrine >0.1 ^b
Central nervous system: Glasgow Coma Scale	15	13–14	10–12	6–9	< 6
Renal: creatinine, mg/dL (micro- mol/L) or urine	<1.2 (<110)	1.2–1.9 (110–170)	2.0–3.4 (171–299)	3.5– 4.9 (300–440) or <500 mL/day	> 5.0 (>440) or <200 mL/day

^aWith ventilatory support.

^bAdrenergic agents administered for at least one hour (doses are given in mcg/kg/min).

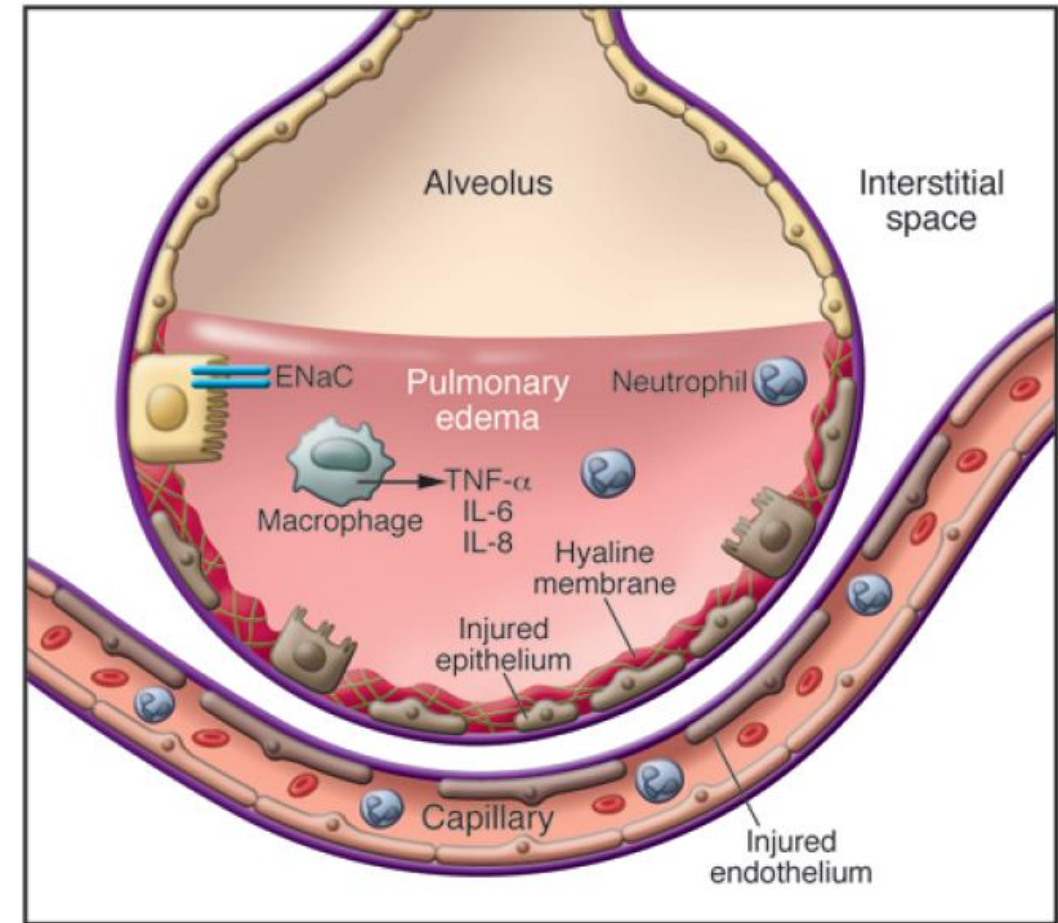


ARDS: The Pulmonary Manifestation of Sepsis

Sepsis is the number 1 risk factor for acute respiratory distress syndrome (ARDS)

ARDS Pathophysiology is defined by:

- Dysregulated inflammation
- Inappropriate accumulation and **activity of leukocytes**
- Uncontrolled coagulation
- Altered **permeability of endothelial** and epithelial barriers of the alveoli

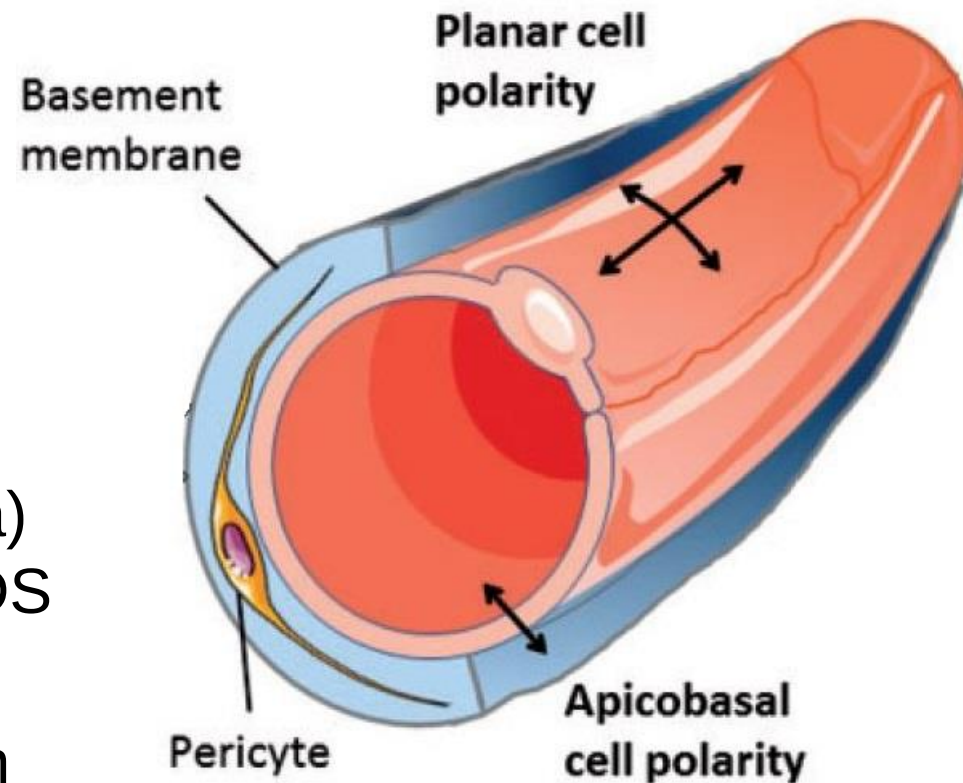


Endothelium Function and Polarity

The pulmonary endothelial cell barrier regulates **leukocyte extravasation** and **edema**

Endothelial cell interactions with inflammatory cytokines (e.g. $\text{TNF-}\alpha$) and pathogen derived endotoxins (e.g. LPS from gram-negative bacteria) can alter these factors, leading to sepsis and ARDS

How do we therapeutically target dysregulation on an endothelial cell level?



Targeting the Immune Response – For Better or For Worse?

LPS (Endotoxin)

Signals through membrane bound Toll-like receptors (**TLR-4**)

Blocking/Transgenic Studies:

- TLR-4 Antagonist
- TLR-4 LOF Mutation
- HA-1A
- J5

Result: Murine resistance to systemic LPS induced sepsis; susceptibility to LPS bearing pathogens

TNF- α (Cytokine)

Signals through membrane bound TNF receptor family (**TNFR1** and TNFR2)

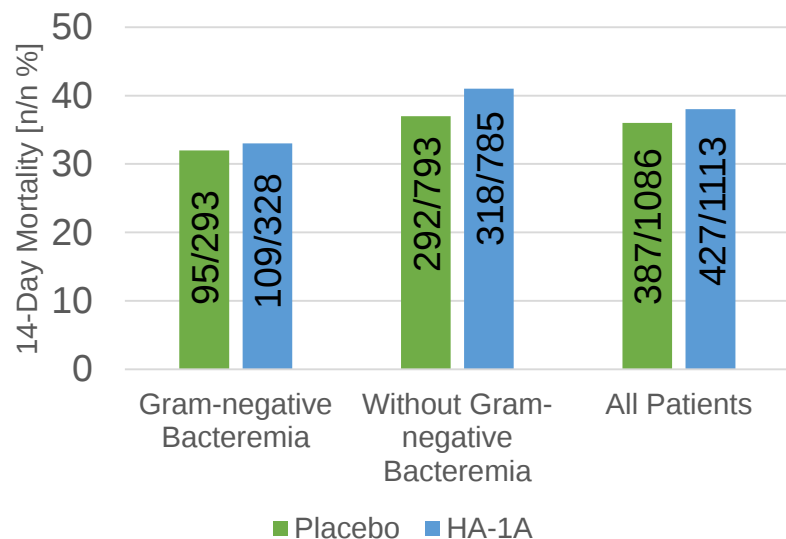
Can be blocked at many levels:

- Systemic (IV Soluble TNFR1)
- Ab (Monoclonal or Polyclonal)
- Receptor Antagonist

Result: Murine resistance to sepsis; high susceptibility to primary (local) infections

Anti-Endotoxin Therapeutics

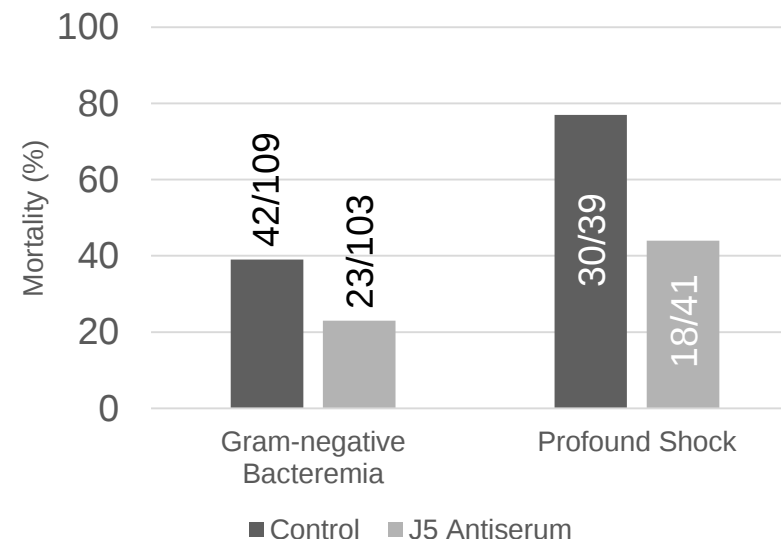
Human Anti-Lipid A Clinical Trails



Conclusion: not effective, inclusion criteria must be reassessed

Graphic adapted from: McCloskey et al., Annals of Internal Medicine 1994

J5 Antiserum (LPS Vaccine)

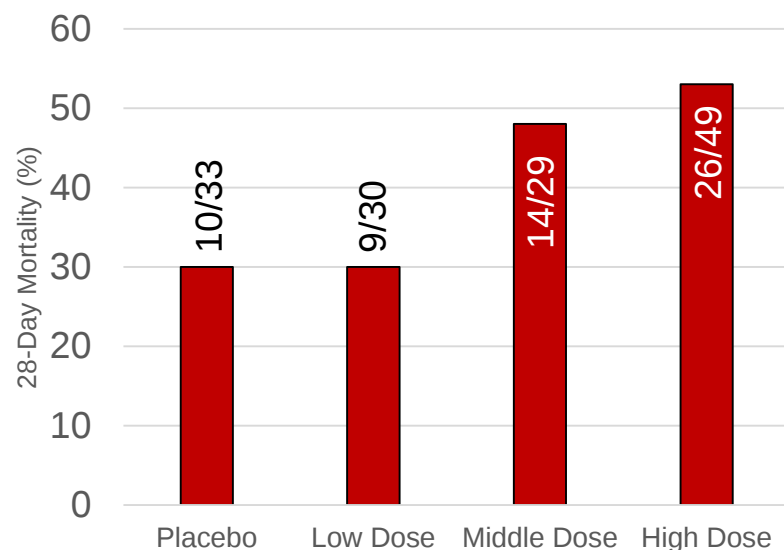


Conclusion: effective; subsequent studies **disprove** results

Graphic adapted from: Ziegler et al., NEJM 1982

Anti-Cytokine Therapeutics

TNFR:Fc Fusion Protein [Etanercept]



Hypothesis: Anti-TNF- α therapy is opening the door for opportunistic pathogens

Conclusion: not effective, may increase mortality?

Graphic adapted from: Fisher et al., NEJM 1996

Overarching Problem

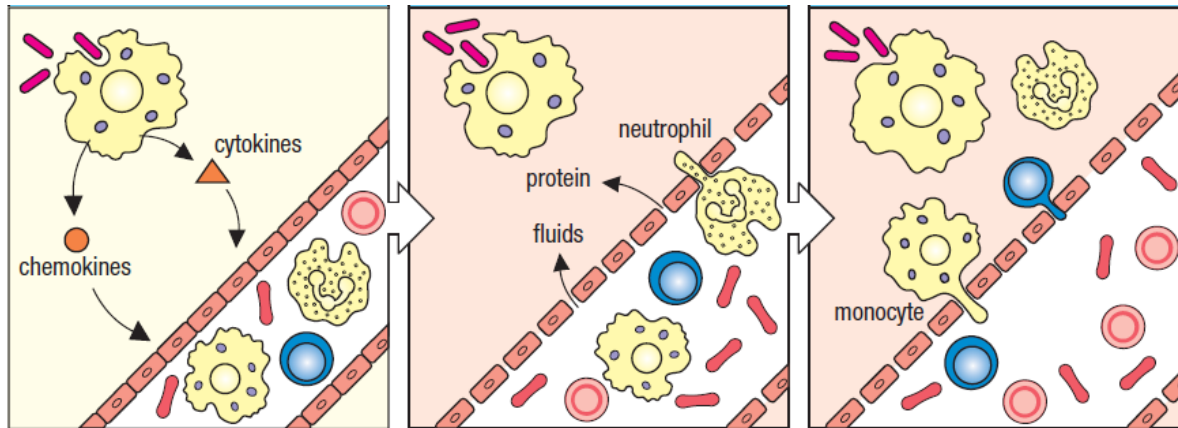
- Sepsis therapeutics, past and present, struggle to balance remedial and pathological immunosuppression
- Developing novel therapeutics *in vivo* is time consuming and expensive

Guiding Hypothesis

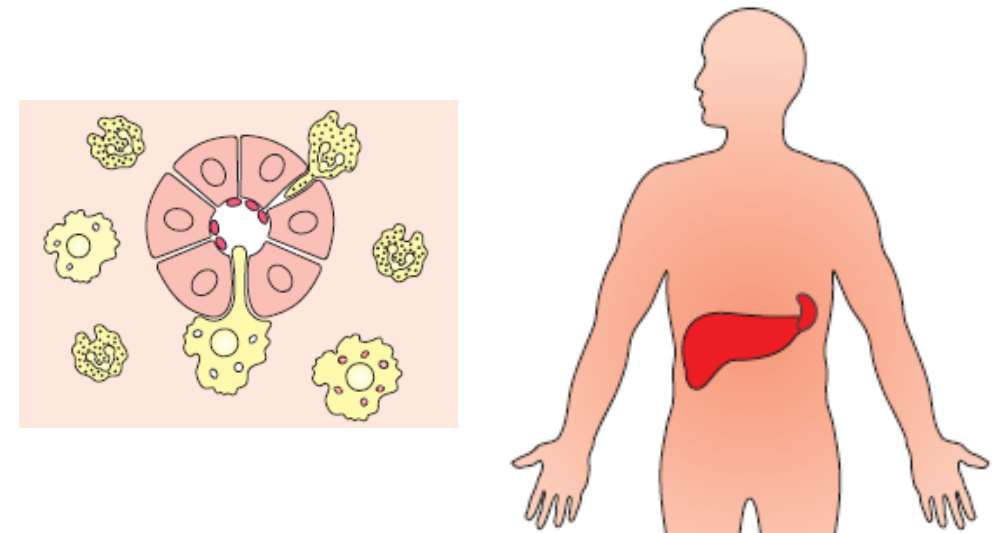
Pulmonary microvasculature mimetics can be utilized to study the distinguishing characteristics of a host response to a **primary infection** versus a **systemic inflammatory response**

Rationale

Local Infection: **Abluminal** Cytokine



Sepsis/SIRS: Systemic/**Luminal** Cytokine



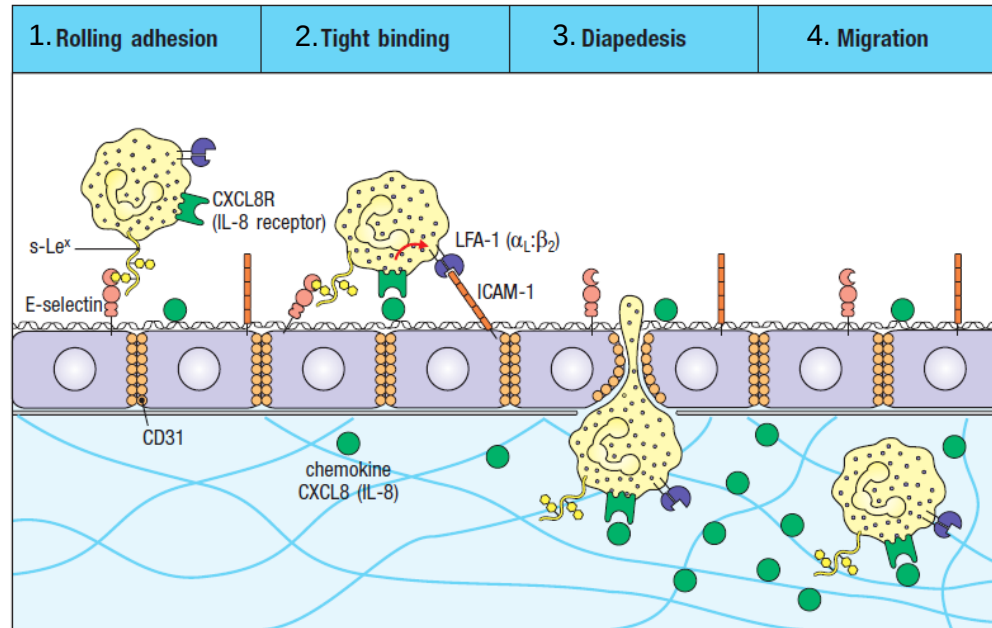
Specific Aims

1. Develop a facile microvasculature mimetic to quantify small molecule and neutrophil permeability in the presence of physiological shear
2. Elucidate the effects of polarized cytokine and endotoxin delivery on neutrophil dynamics and endothelial cell biology
3. Demonstrate the polarized dependence of S1P in regulating pulmonary vasculature permeability and neutrophil dynamics following septic insult *in vitro*

Specific Aims

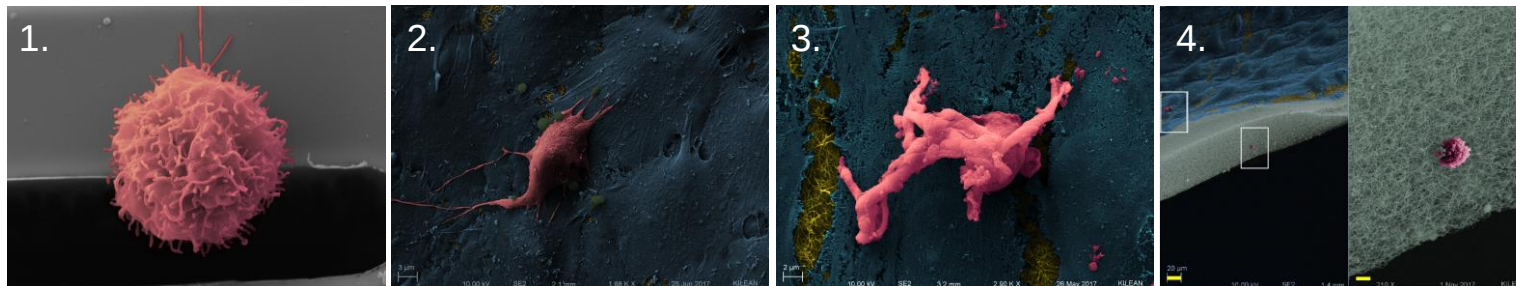
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3. Demonstrate the polarized dependence of S1P in regulating pulmonary vasculature permeability and neutrophil dynamics following septic insult *in vitro*

Bringing the Pulmonary Microvasculature to the Lab Bench¹⁴

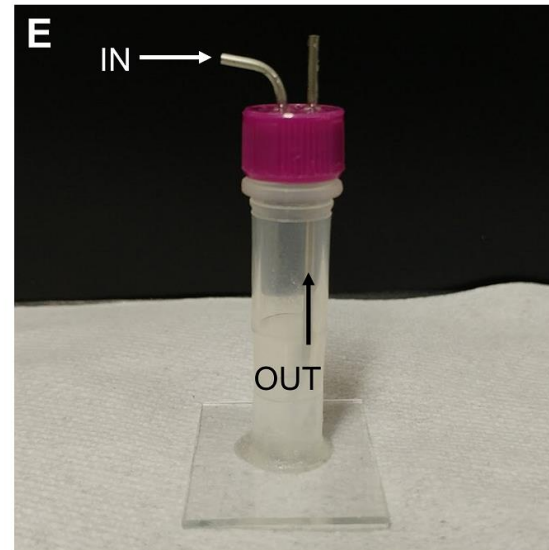
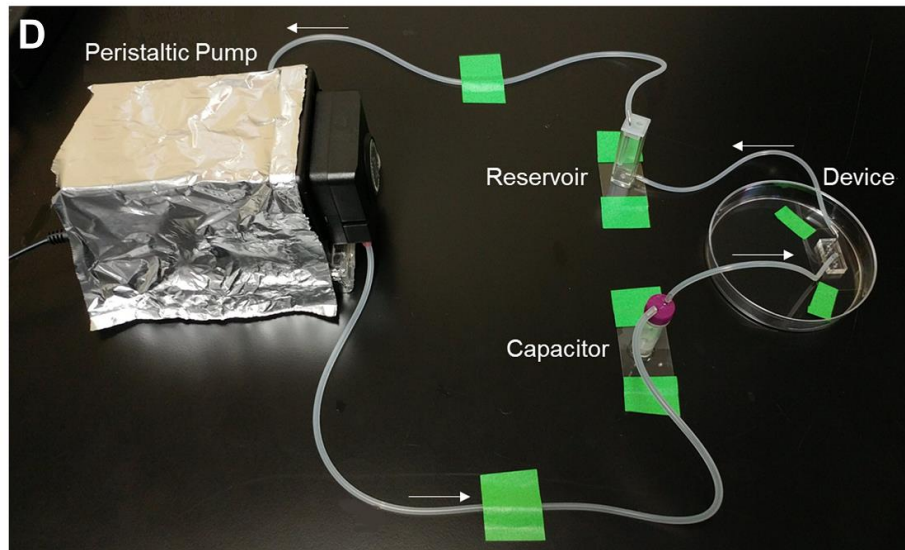
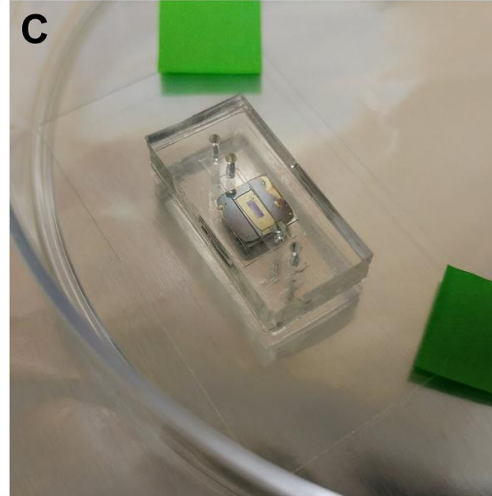
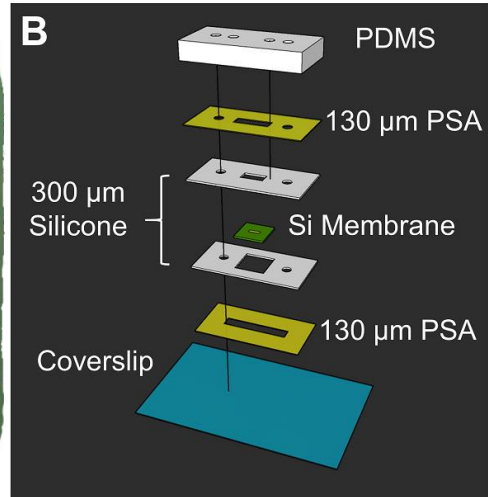
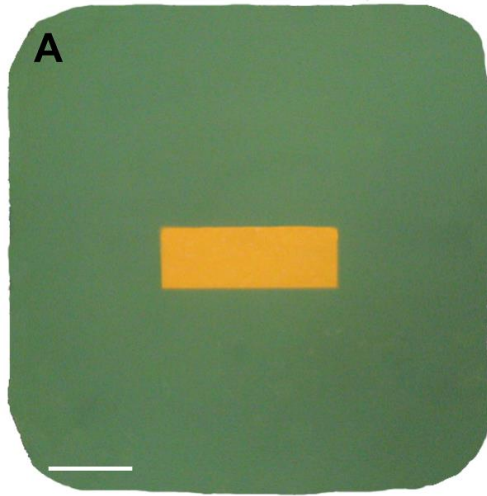


Success Metrics

- I. Contain defined luminal and abluminal media compartments
- II. Allow for shear priming of microvascular endothelial cells on a porous substrate
- III. Permit phase contrast tracking of live PMNs
- IV. Facilitate continuous *in situ* permeability measurements

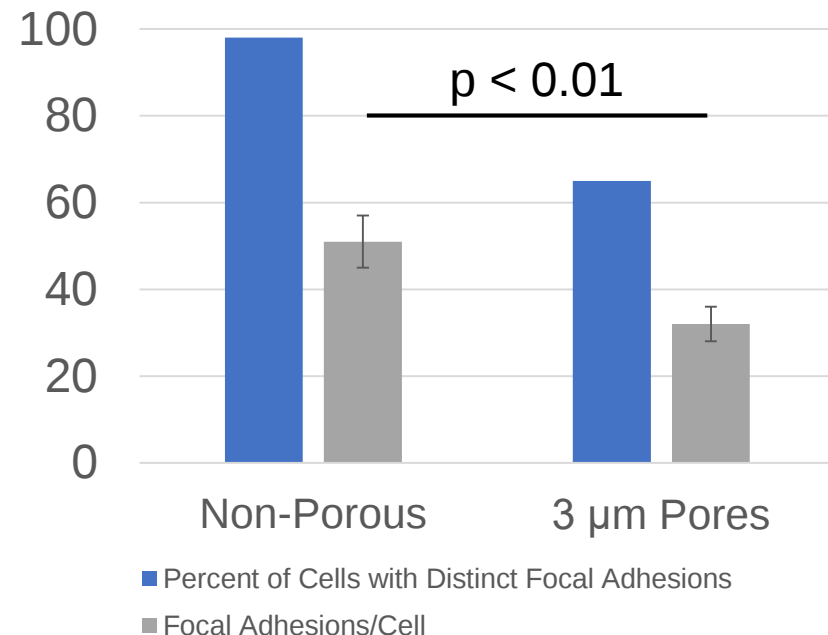
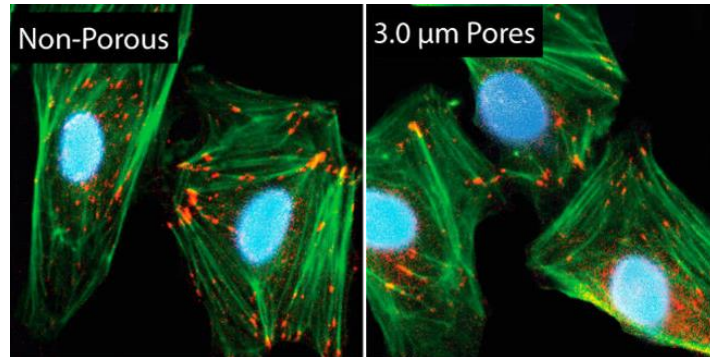


μ SiM-PVB: Microfluidic Silicon Membrane Enabled Pulmonary Vascular Barrier ¹⁵



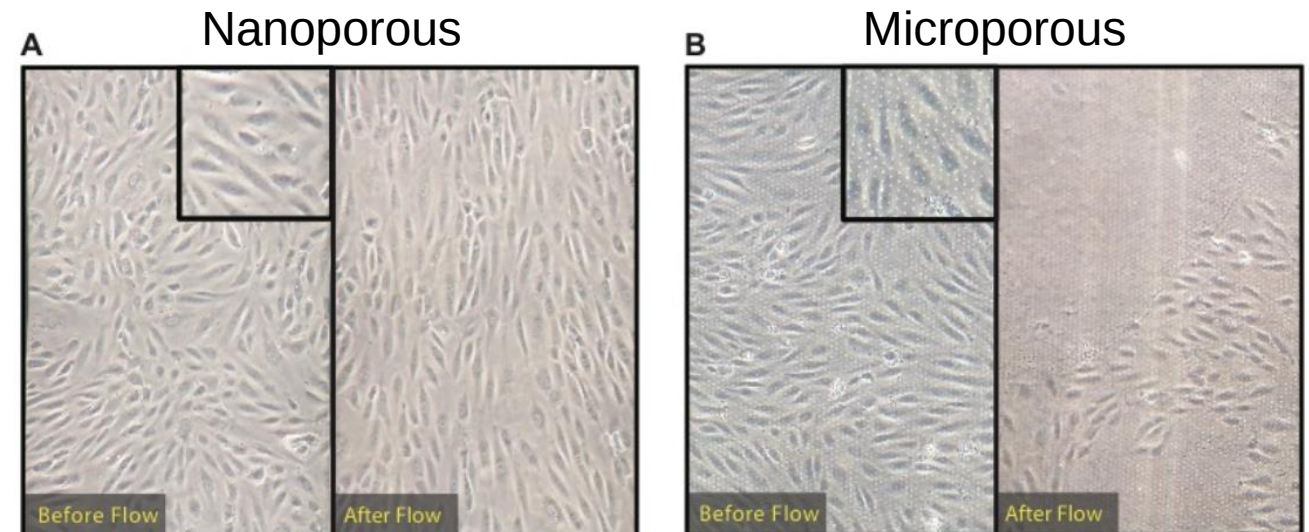
- ✓ Silicon membranes enable phase contrast imaging
- ✓ Layer-by-layer fluidic assembly features defined luminal and abluminal channels
- ✓ Custom flow circuit permits bubble-free shear priming of cells

Cell Culture on Microporous Substrates

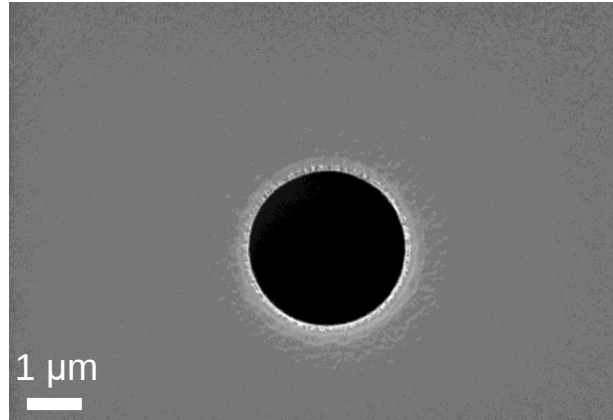
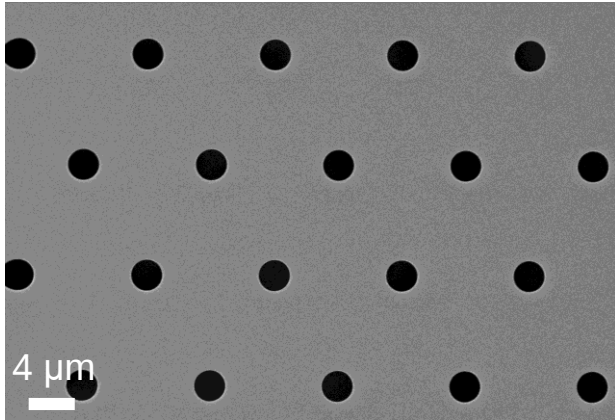


A silicon nanomembrane platform for the visualization of immune cell trafficking across the human blood–brain barrier under flow

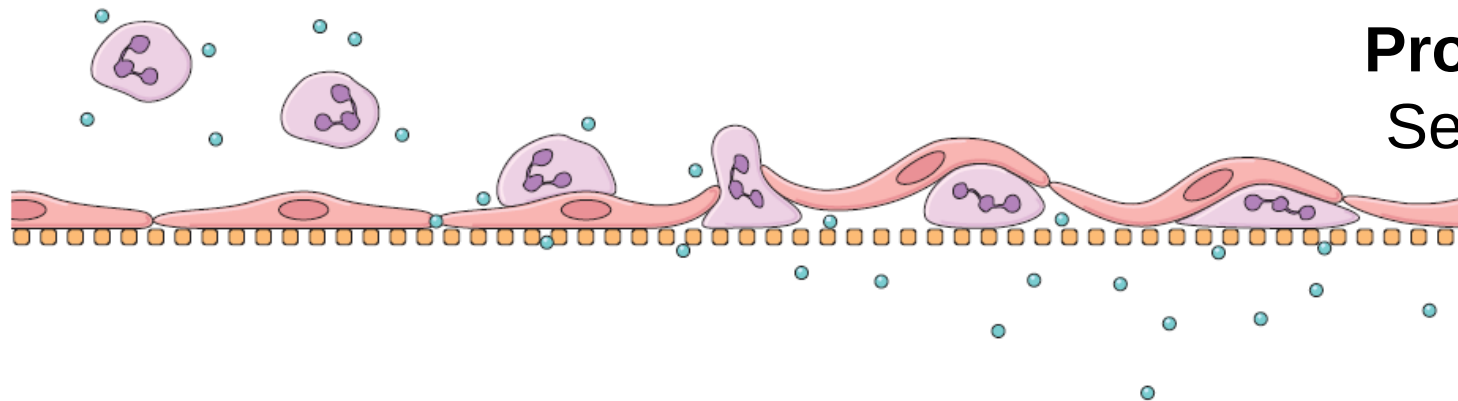
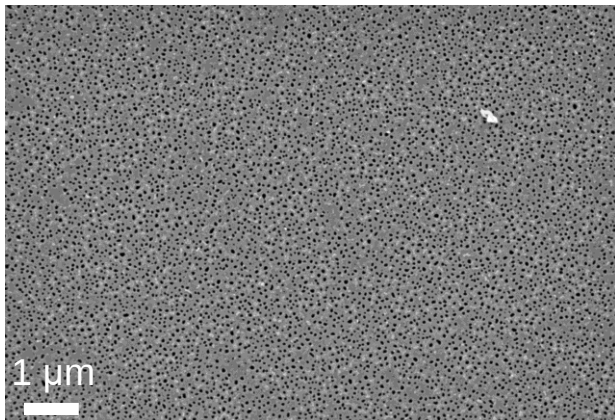
Adrien Mossu^{1,*}, Maria Rosito^{1,*}, Tejas Khire², Hung Li Chung², Hideaki Nishihara¹, Isabelle Gruber¹, Emma Luke², Lucie Dehouck³, Federica Sallusto^{4,5}, Fabien Gosselet³, James L McGrath² and Britta Engelhardt¹



Membrane Cell Culture Paradox



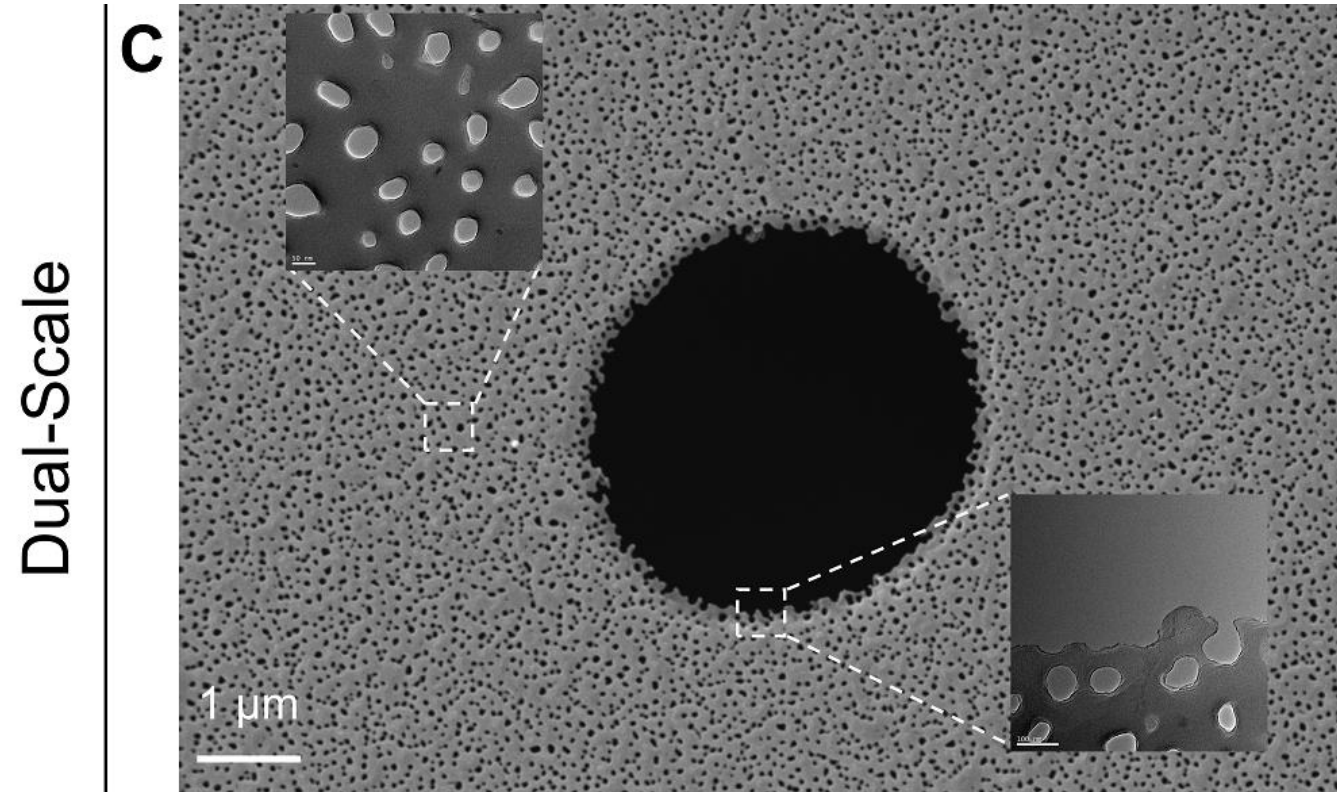
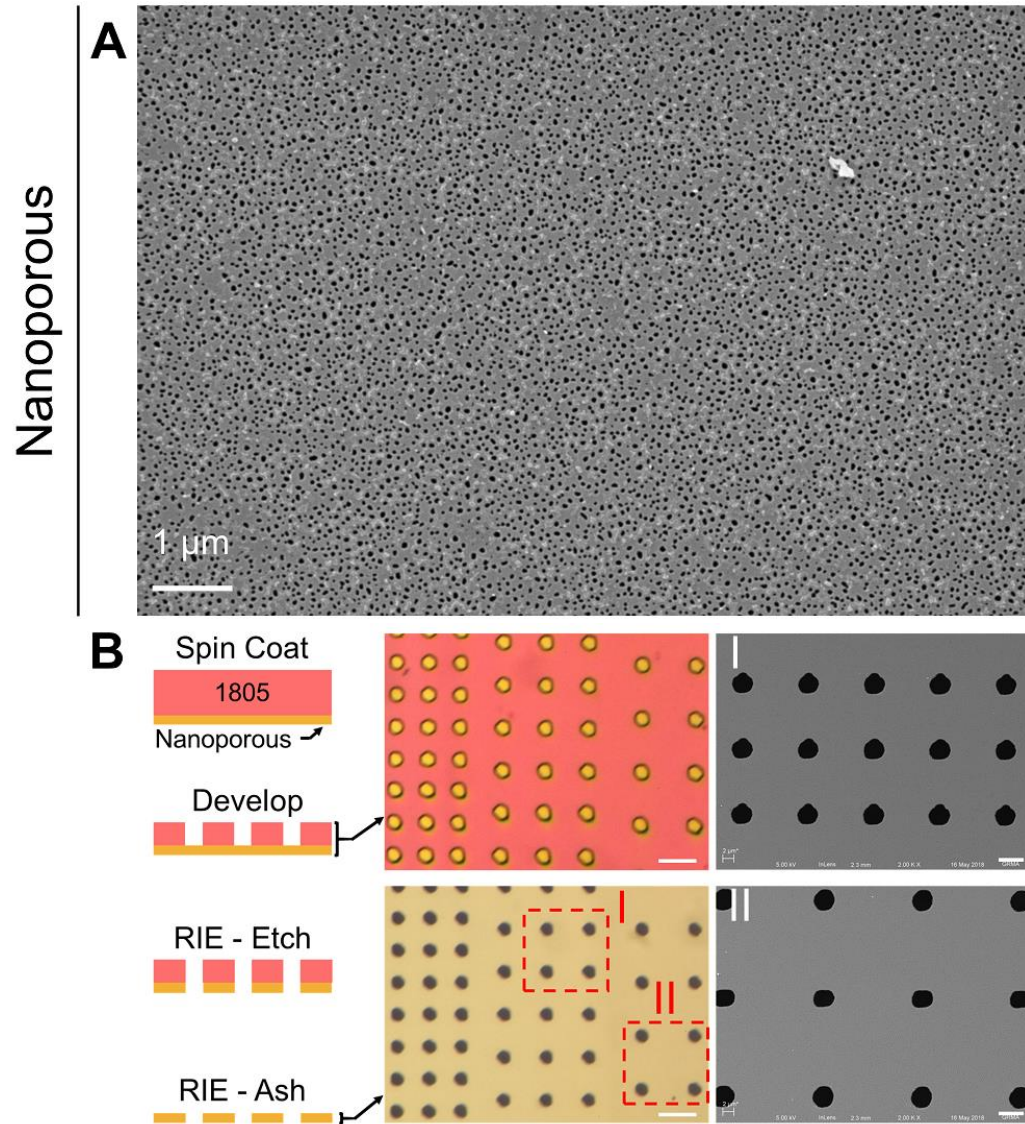
Problem: Cell loss under physiological shear



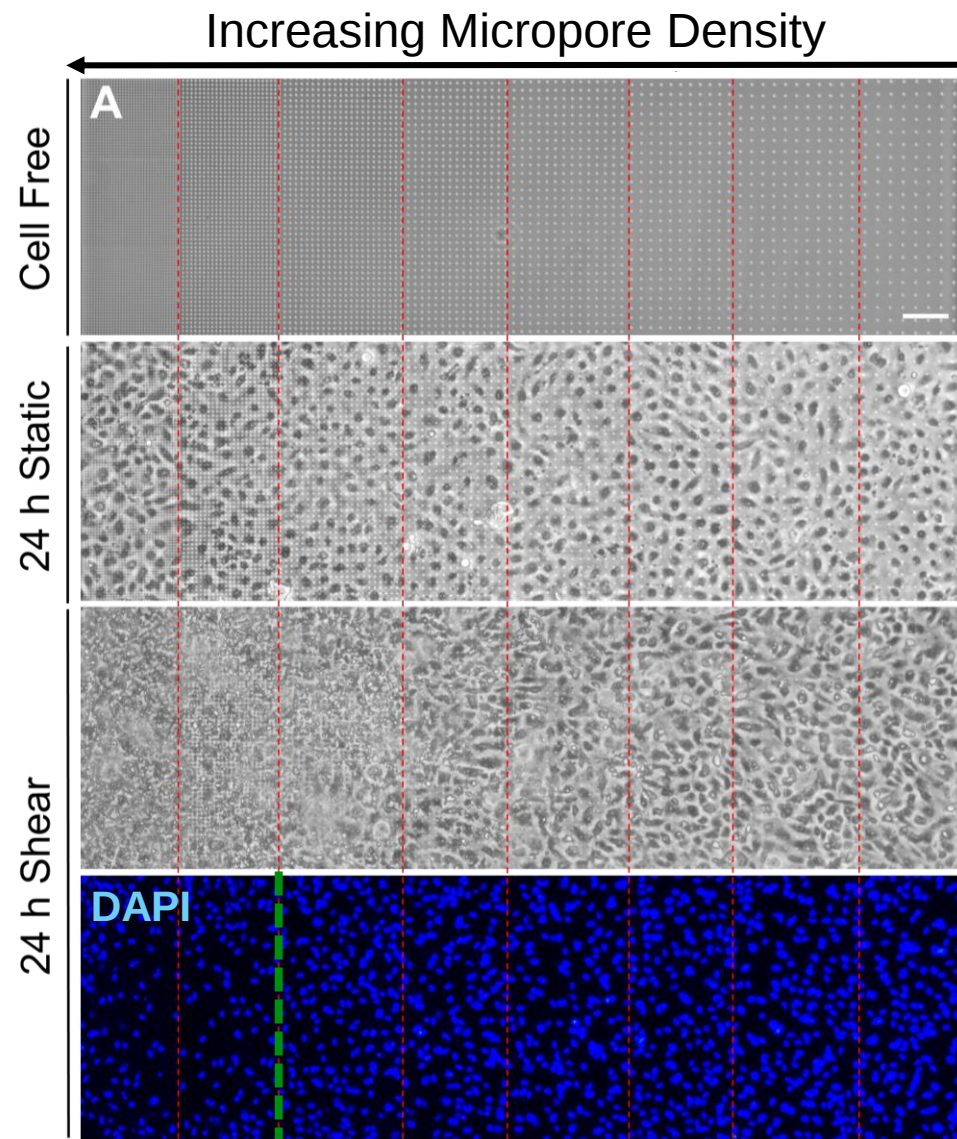
Problem: PMN Sequestration

Solution: Hierarchical pore membranes will permit abundant cell-substrate interactions without reducing permeability

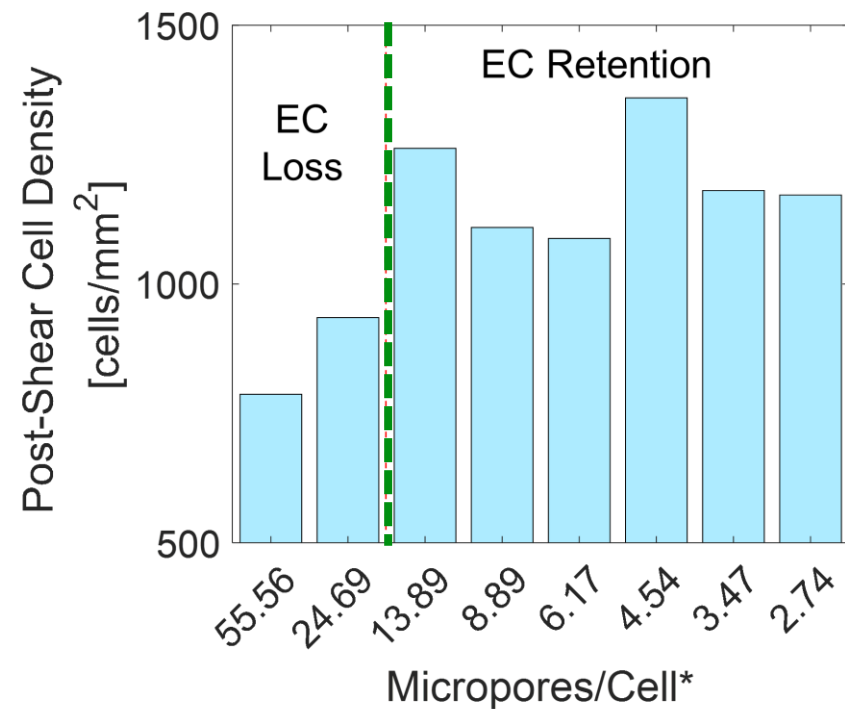
Dual-Scale (Nano- and Microporous) Membranes

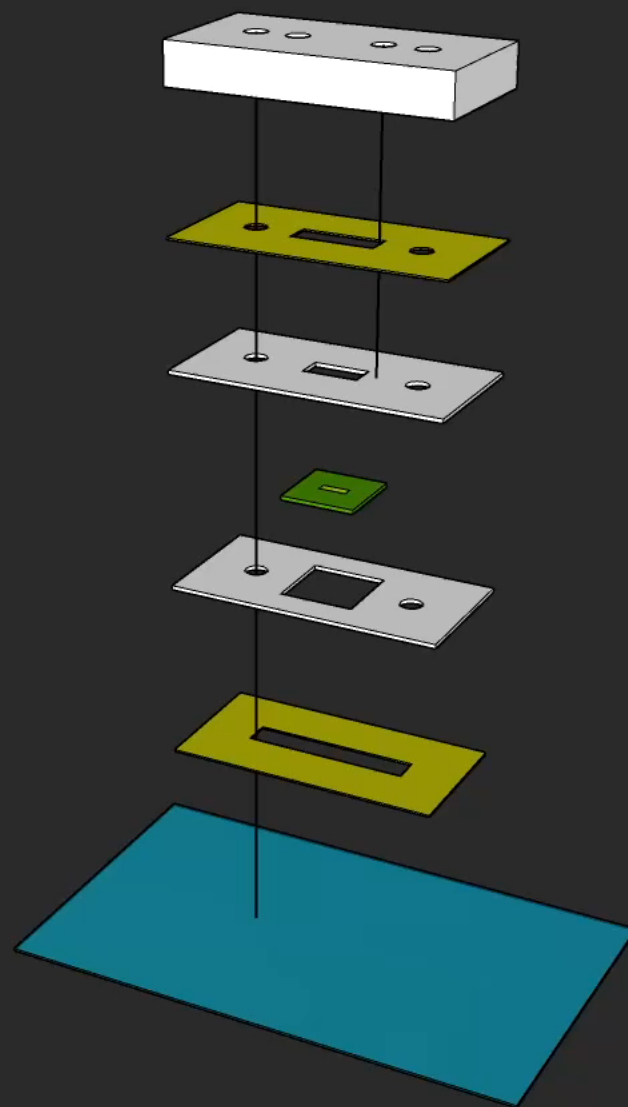


Cell Culture on Dual-Scale Membranes

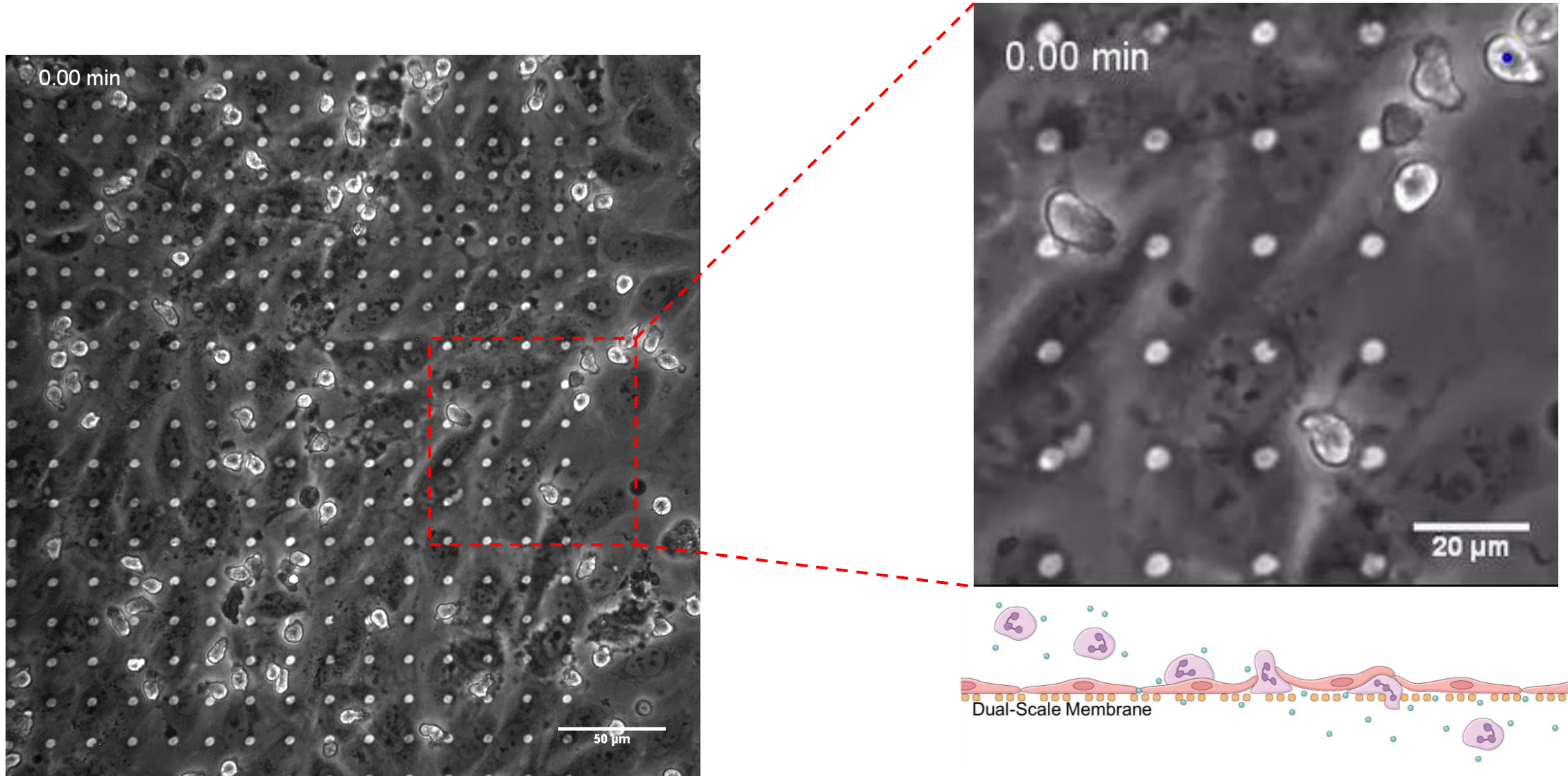


C



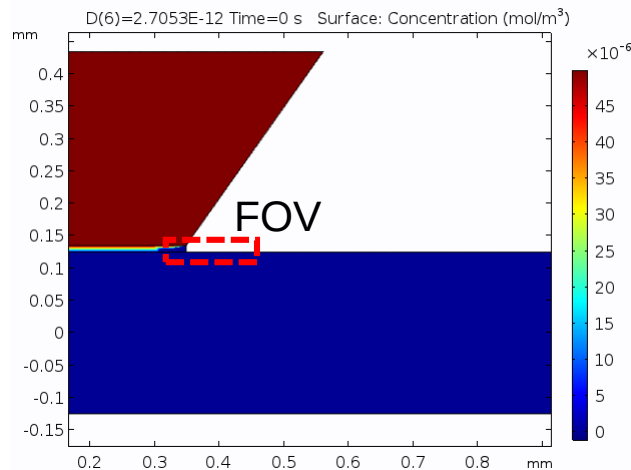


Dual-Scale Membranes Permit PMN Tracking

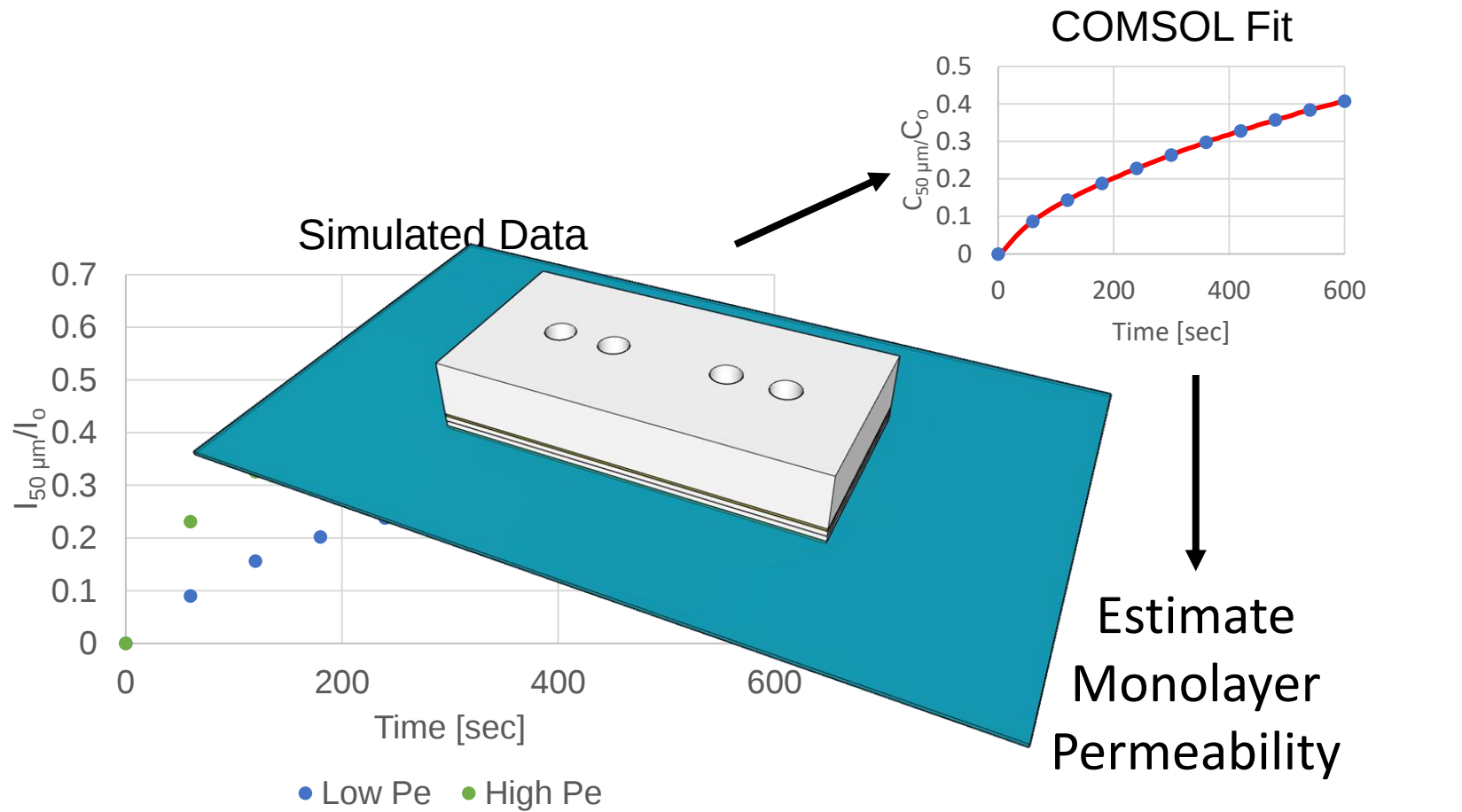
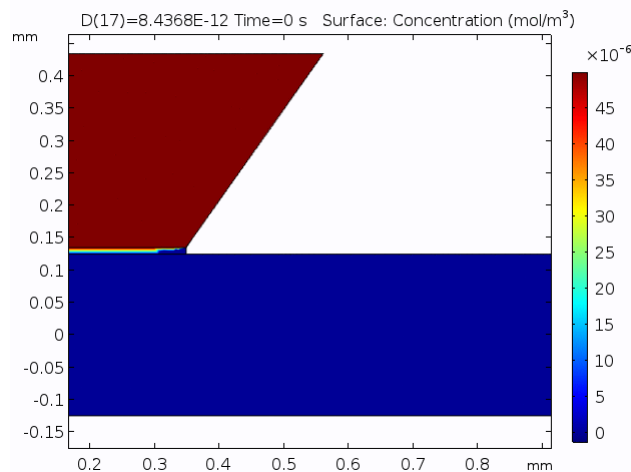


In Situ EC Permeability Assay

Low Permeability
'Healthy Monolayer'

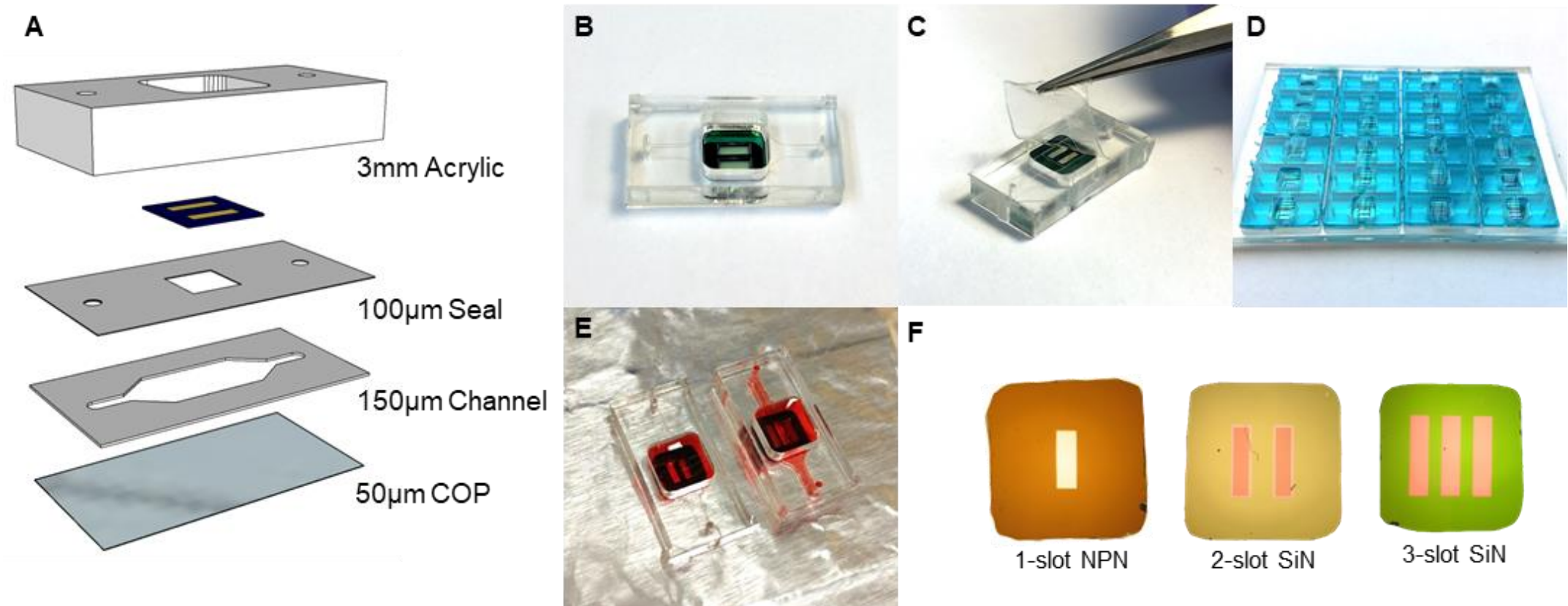


High Permeability
'Septic Monolayer'

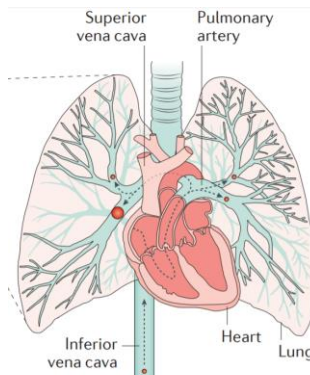
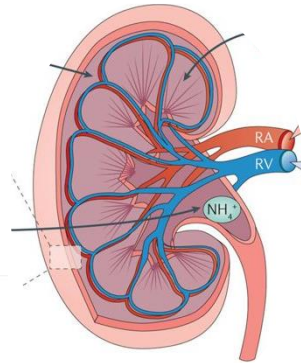
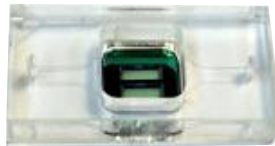
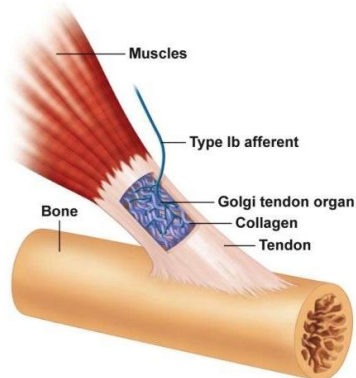
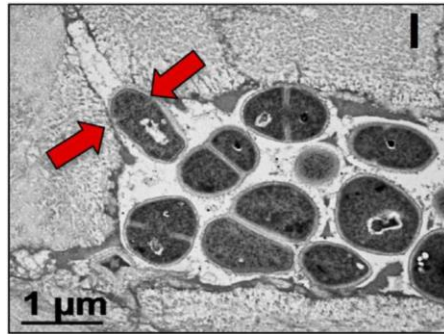
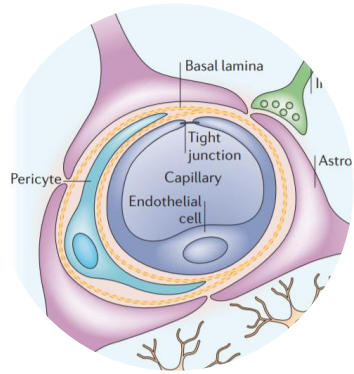


$$\frac{1}{P_{EC}} = \frac{x}{D} - \left[\frac{1}{P_{NPN}} + \frac{L}{D_{dextran}} \right]$$

High-Throughput Manufacturing

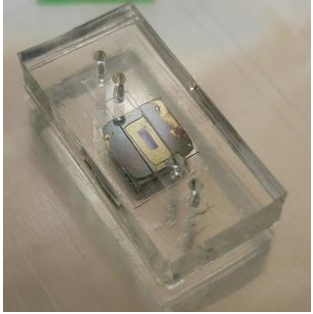


Supporting Collaborations Through High-Throughput Manufacturing

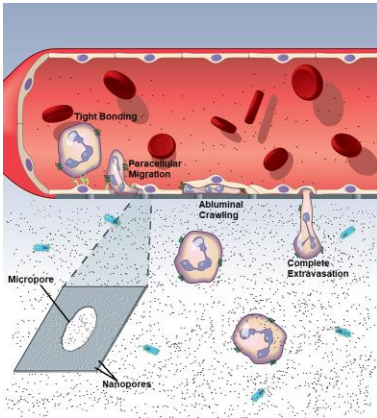


- I. Dr. Edward Schwarz – University of Rochester, Rochester, NY; Microfluidic Silicon Membrane Enabled **Canalicular Array** (μ SiM-CA)
- II. Dr. Britta Engelhardt – University of Bern, Bern, Switzerland; μ SiM- **Blood Brain Barrier** (BBB)
- III. Dr. Angela Glading – University of Rochester, Rochester, NY; Microvasculature
- IV. Dr. Itzik Cooper – Sheba Medical Center, Ramat Gan, Israel; BBB
- V. Daan Hart – Radboud University Medical Center, Nijmegen, Netherlands; Podocyte Culture (**Kidney** on a chip)
- VI. Dr. Diana Hudecz – Aarhus University, Aarhus C, Denmark; BBB
- VII. Dr. Hani Awad – University of Rochester, Rochester, NY; **Tendon/Bone** Fibroblast Culture

Aim 1 Summary



- ✓ Designed and built a ready-to-use microfluidic system to mimic the PVB



- ✓ Fabricated novel dual-scale membrane that permits EC adherence and phase tracking of PMNs

- ✓ *In Situ* permeability measurements

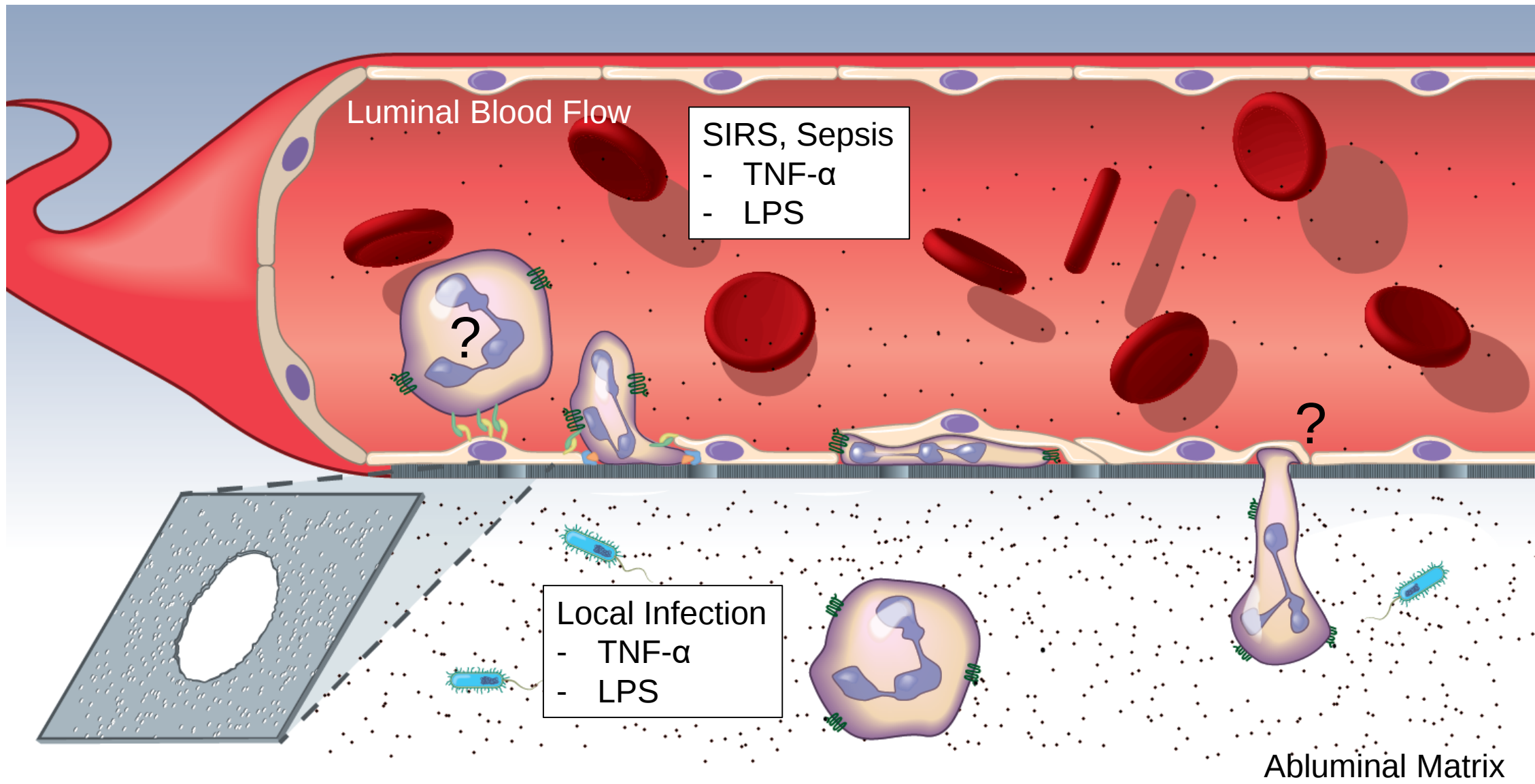


- ✓ High-Throughput manufacturing

Specific Aims

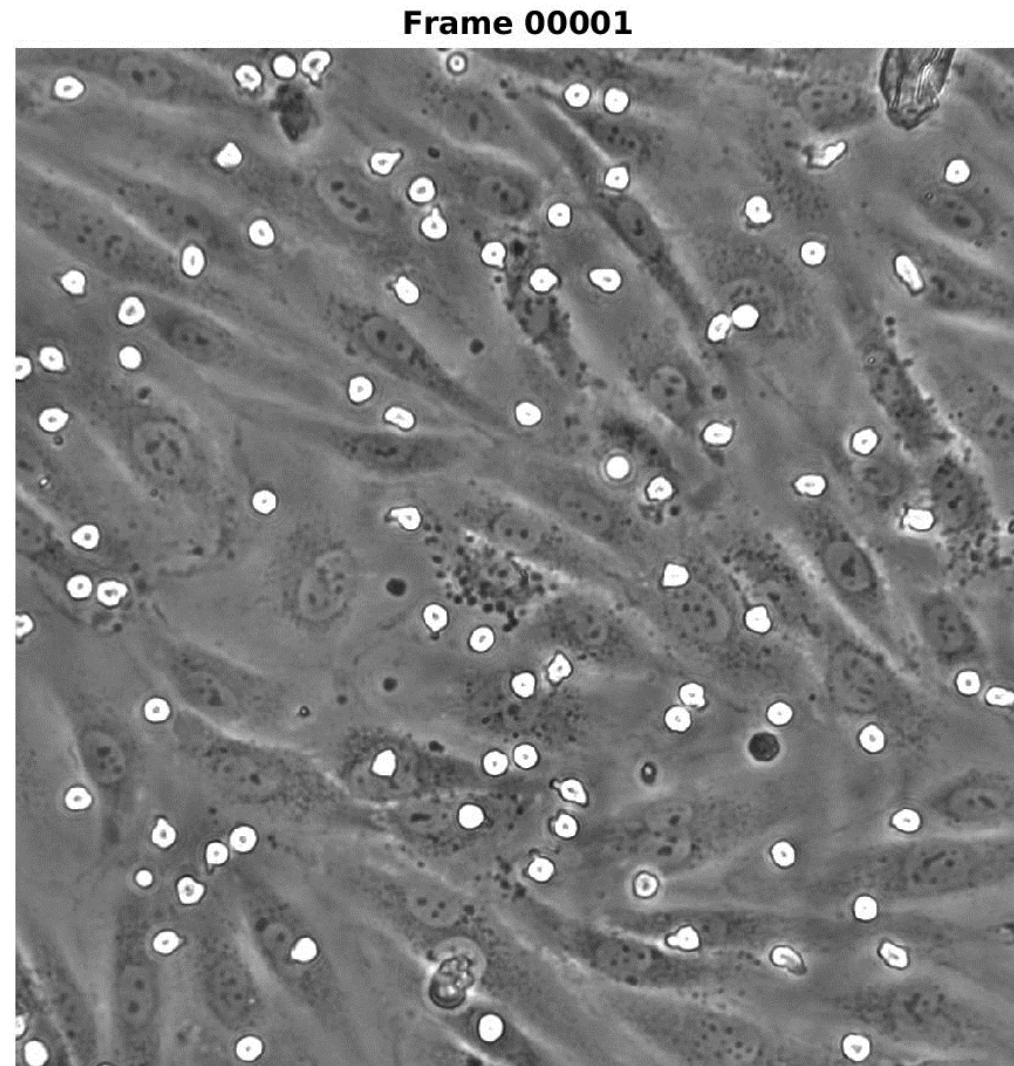
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3. Demonstrate the polarized dependence of S1P in regulating pulmonary vasculature permeability and neutrophil dynamics following septic insult *in vitro*

Systemic Inflammation vs. Local Infection



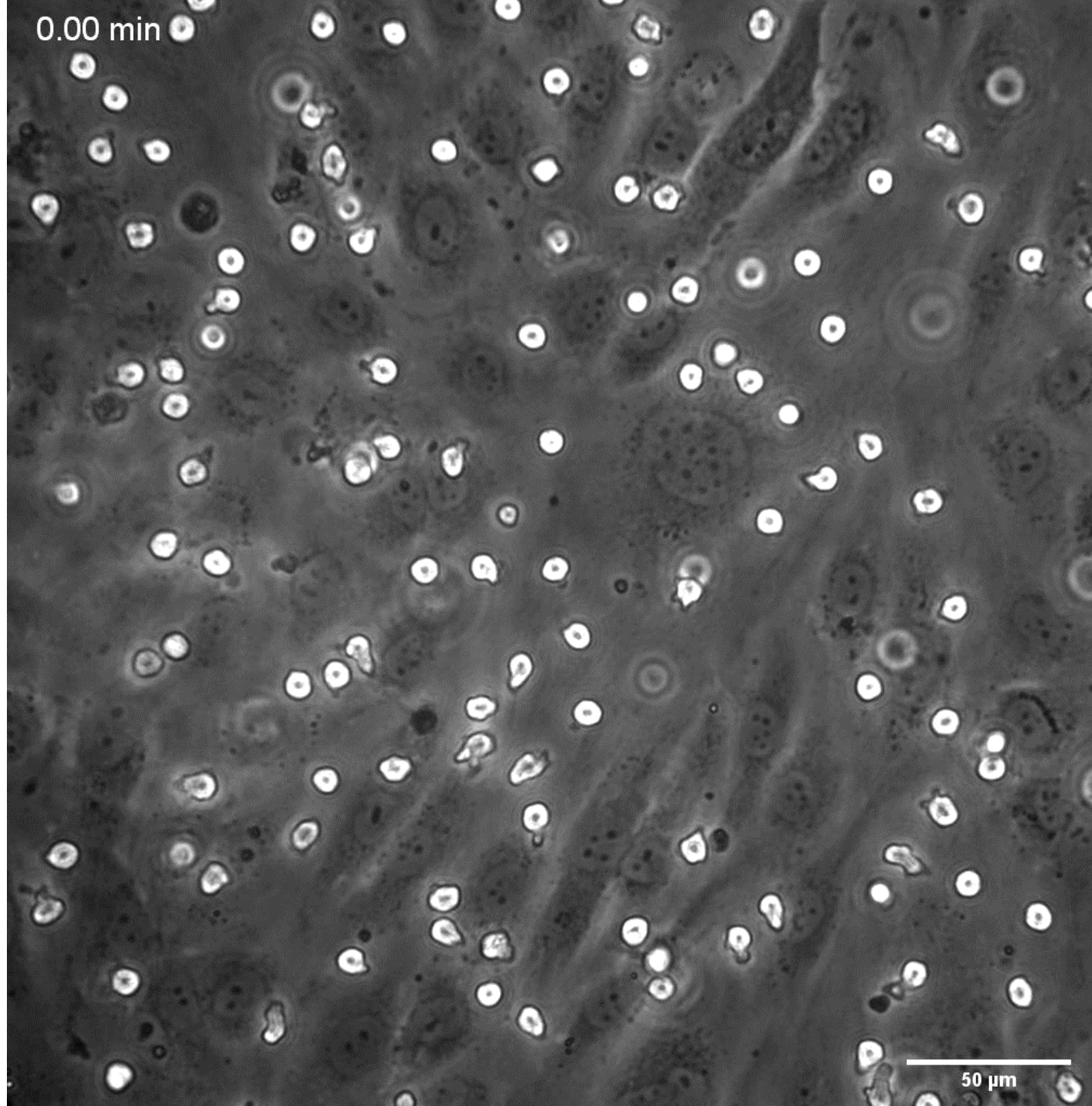
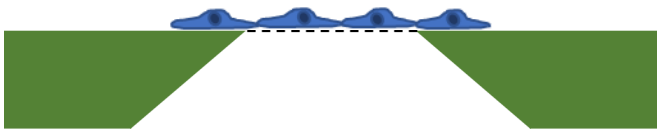
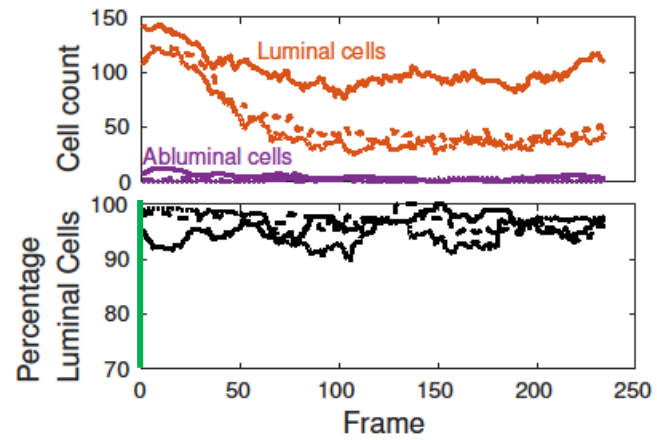
Automated Leukocyte Tracking

- A previously established **particle tracking algorithm** will be adapted for tracking neutrophils [Kelley Lab, University of Rochester]
- Phase contrast movies allow for **pixel intensity tracking** of luminal and abluminal leukocyte dynamics, as well as diapedesis events
- **Unbiased** quantification of leukocyte immune response

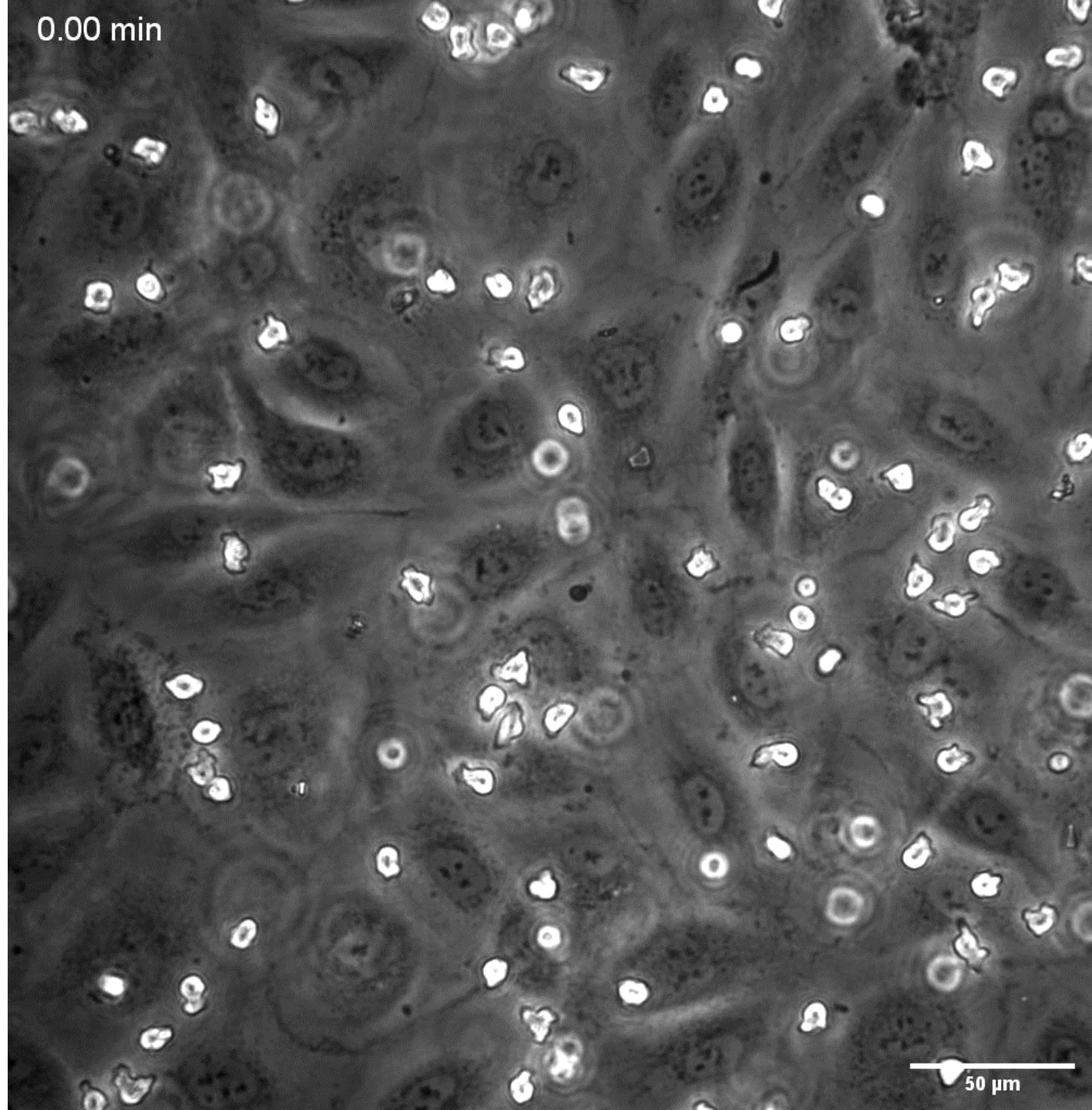
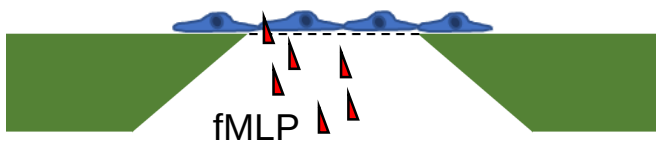
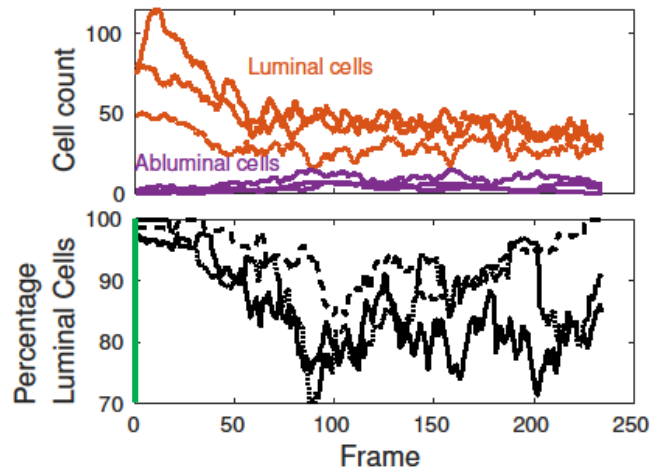


Elapsed 30 min

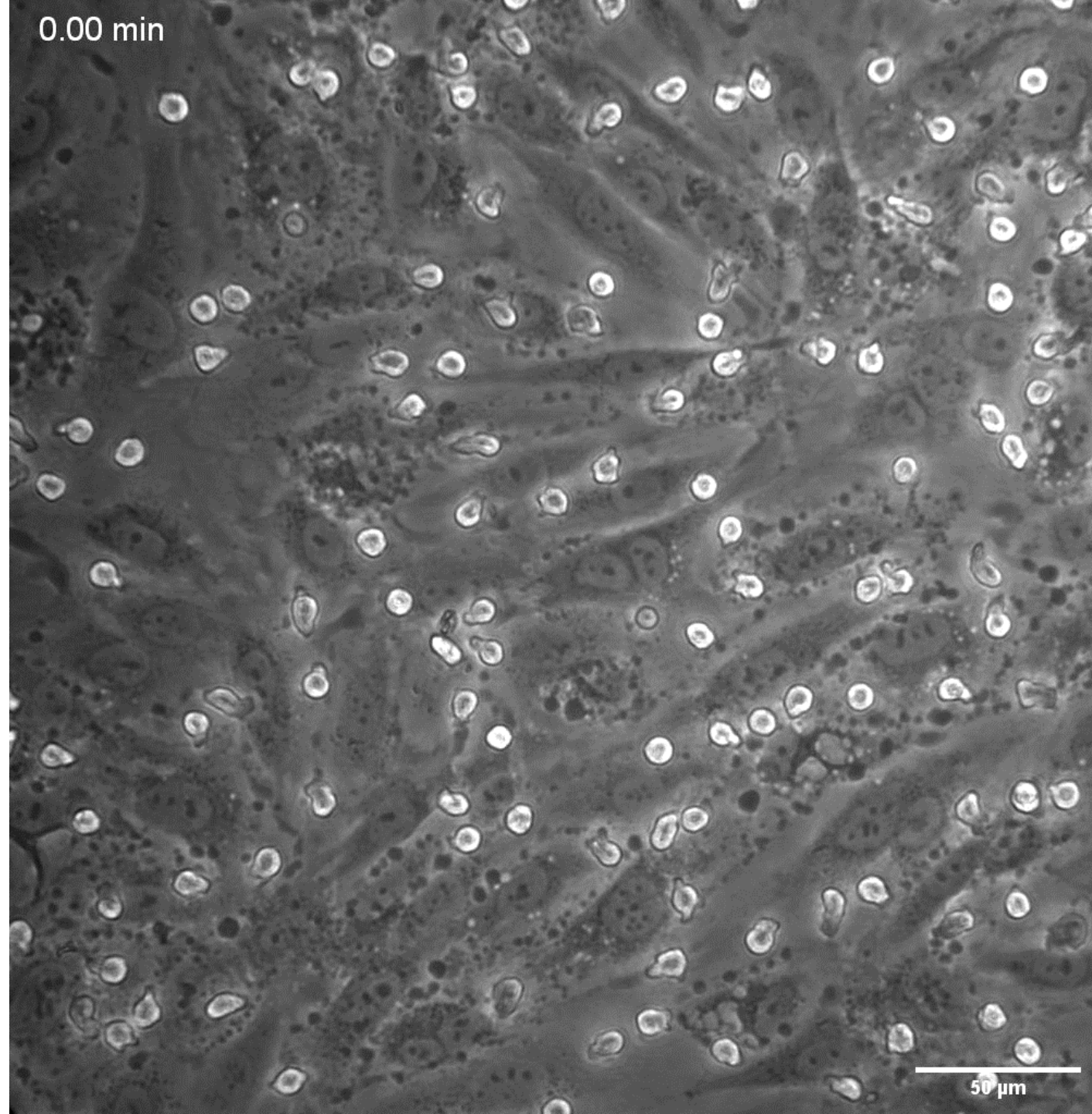
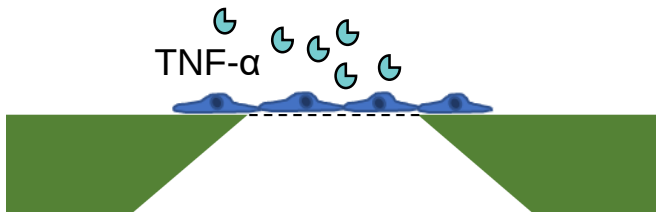
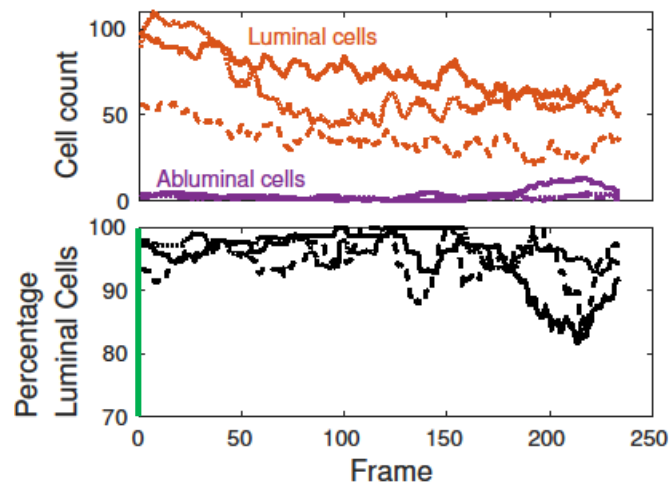
Negative Control –
Neutrophils isolated
from healthy donors on
unstimulated HUVECs



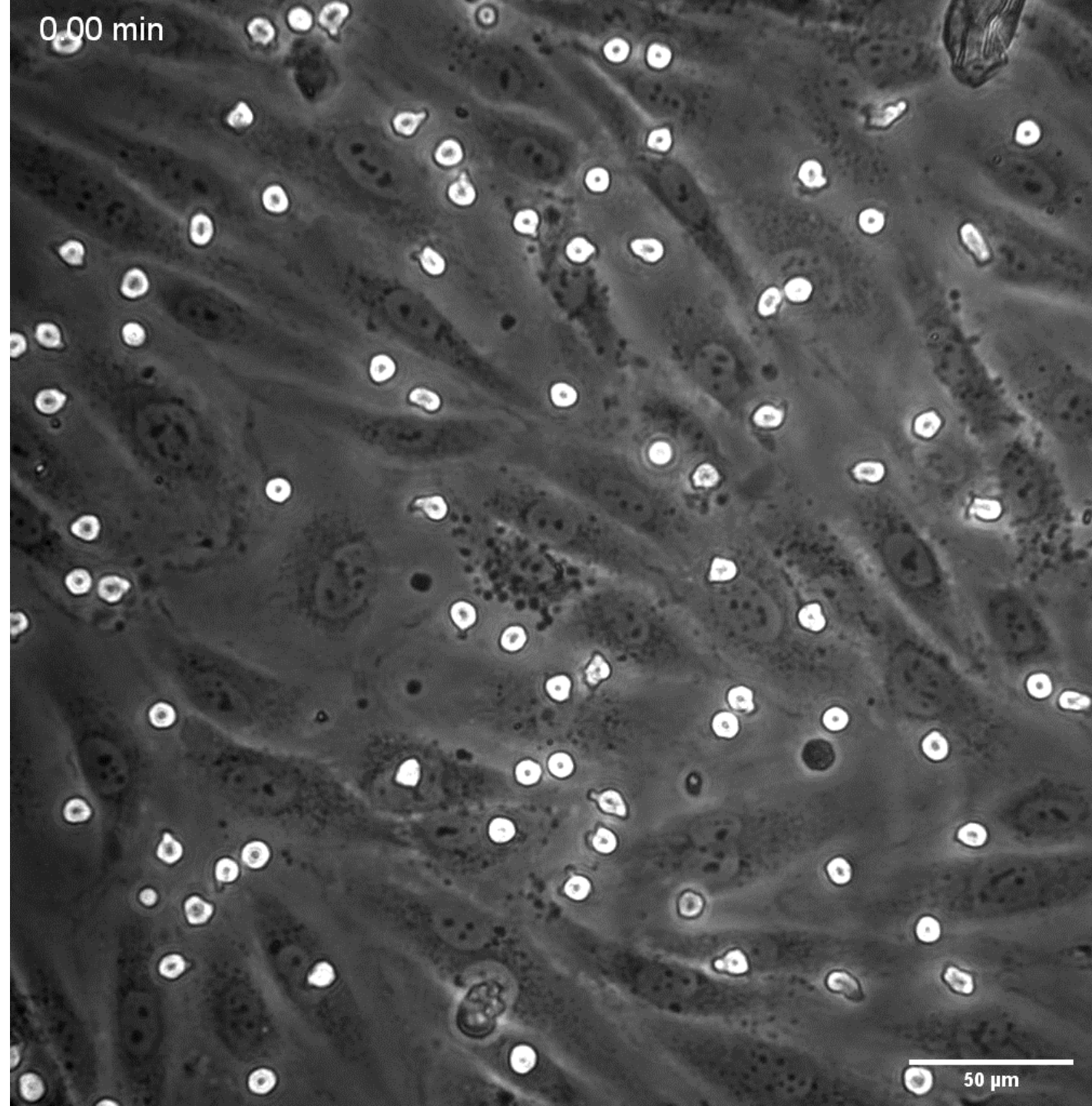
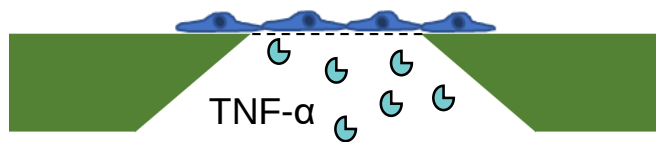
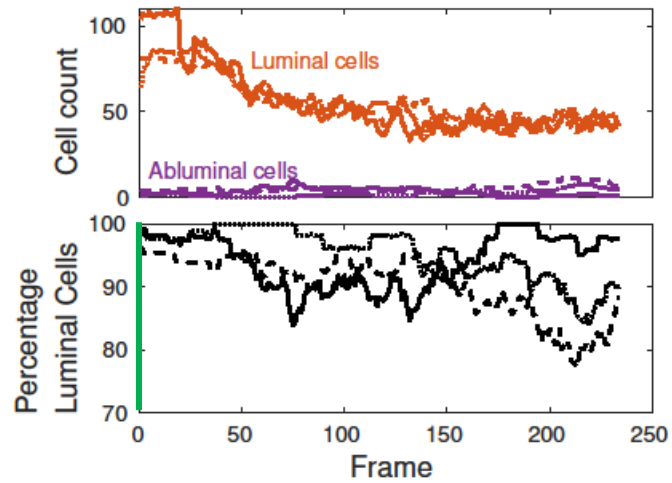
Positive Control –
Neutrophils on
unstimulated HUVECs
with a fMLP gradient



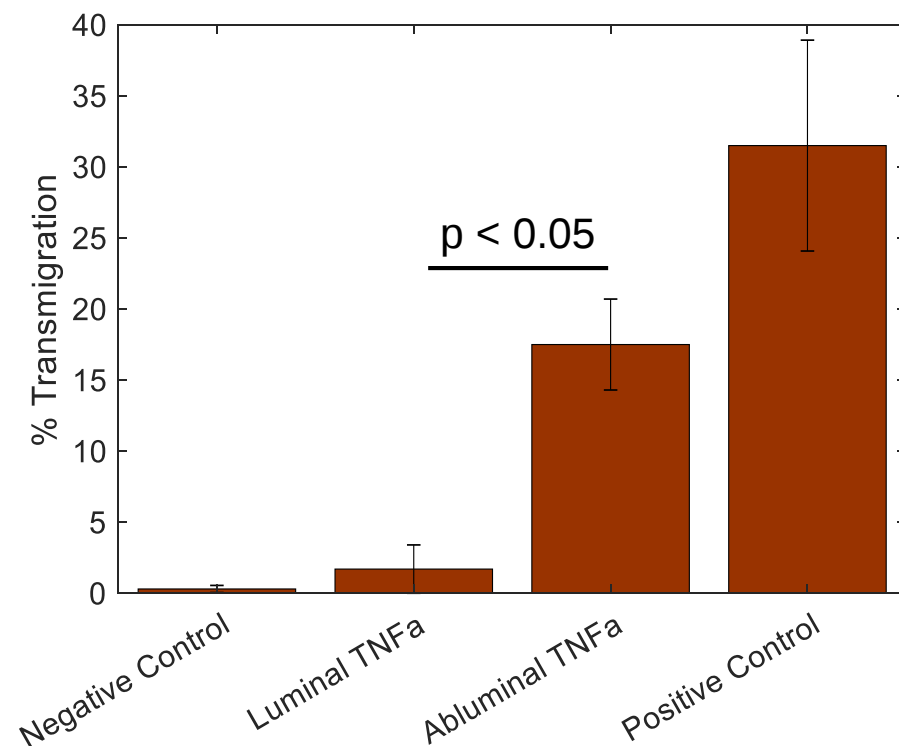
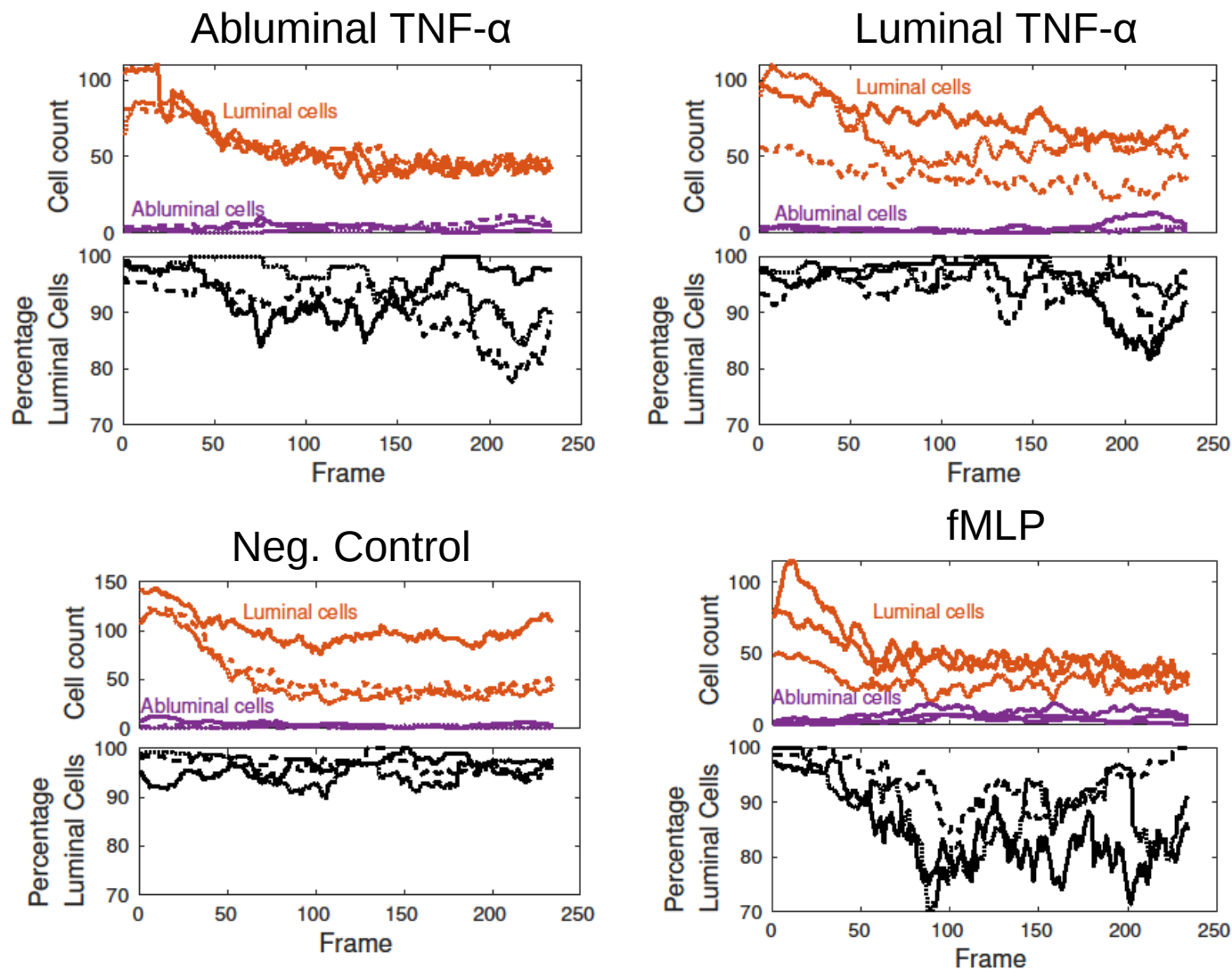
Luminal TNF- α –
Neutrophils on luminally
stimulated HUVECs (20
ng/mL TNF- α for 24 h)



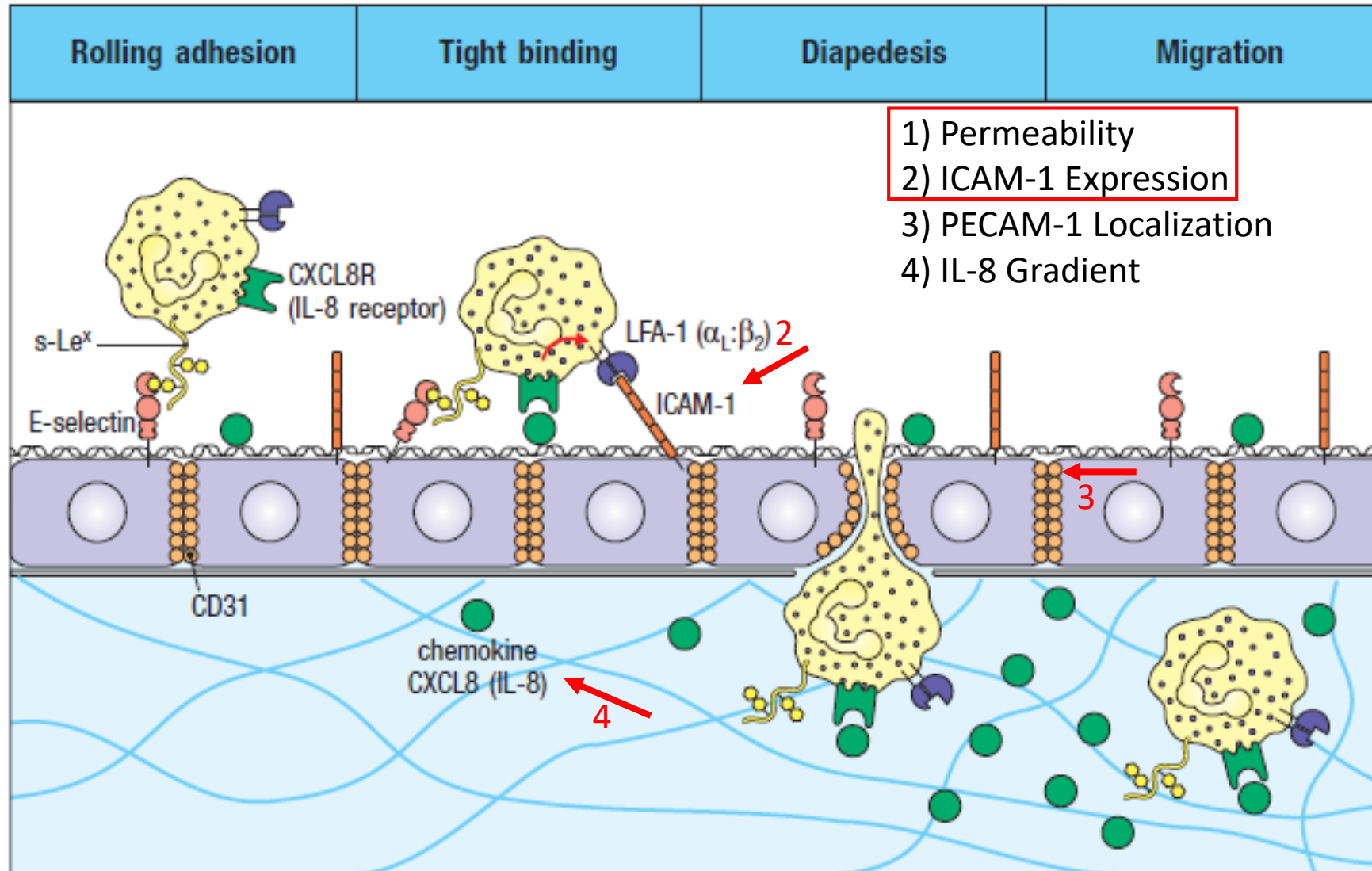
Abluminal TNF- α –
Neutrophils on
abluminally stimulated
HUVECs (20 ng/mL
TNF- α for 24 h)



Abluminal TNF- α Induces a Potent PMN Response



Response Mechanism



- 1) Permeability
- 2) ICAM-1 Expression
- 3) PECAM-1 Localization
- 4) IL-8 Gradient

Enhanced Diapedesis Response to Abluminal TNF α is independent of ICAM-1 and EC Permeability³⁵

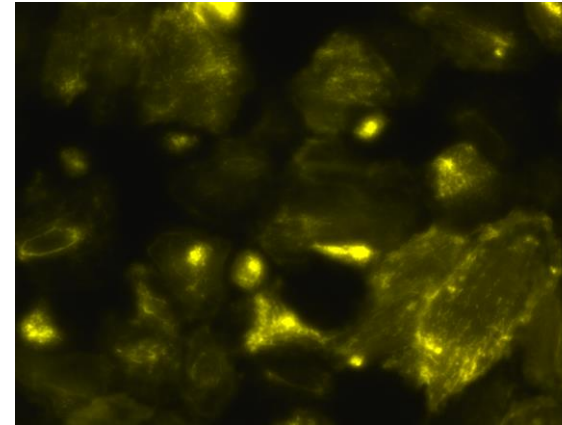
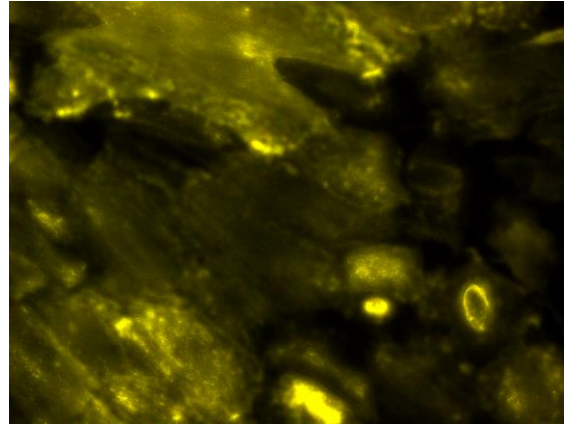
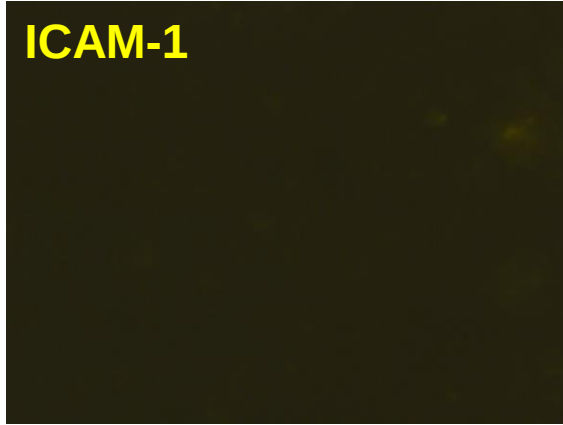
A

Control

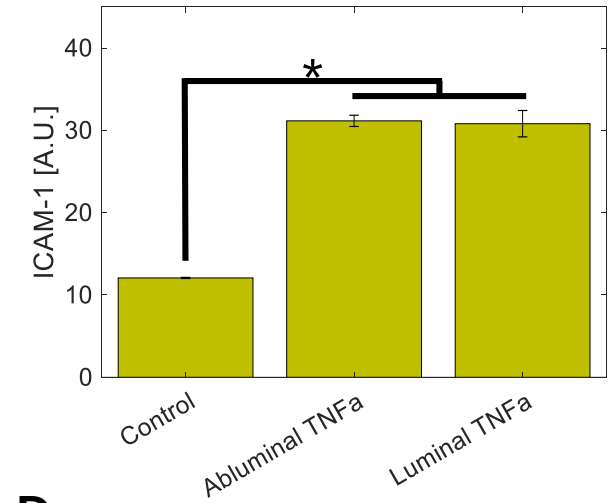
Abluminal TNF α

Luminal TNF α

ICAM-1

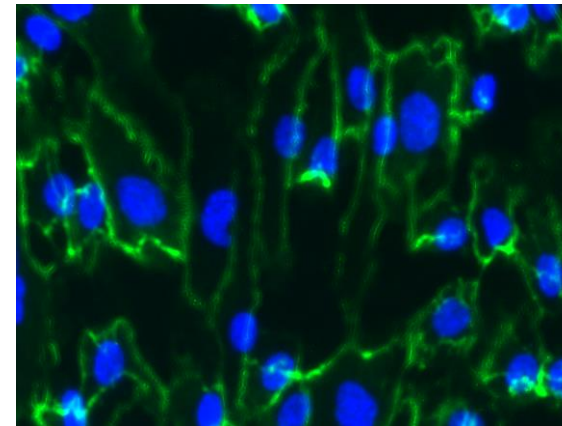
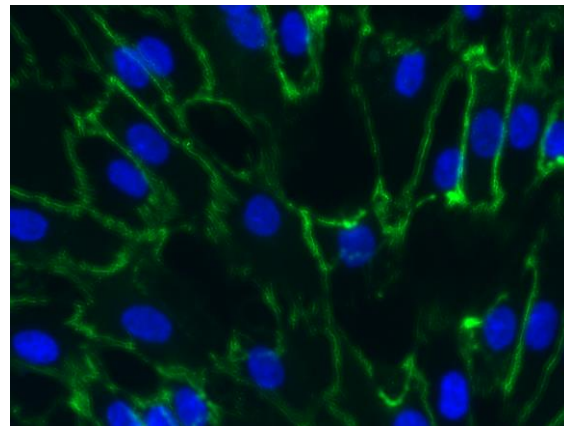
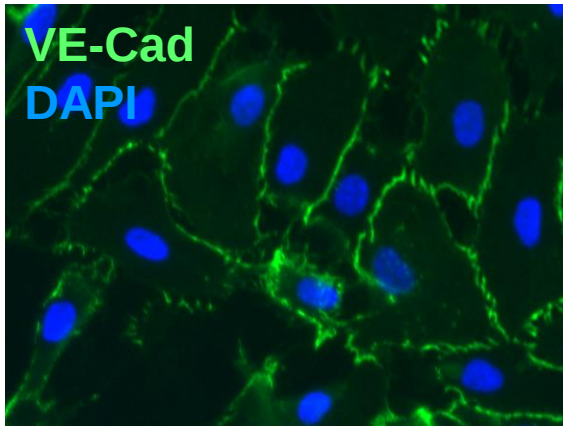


B

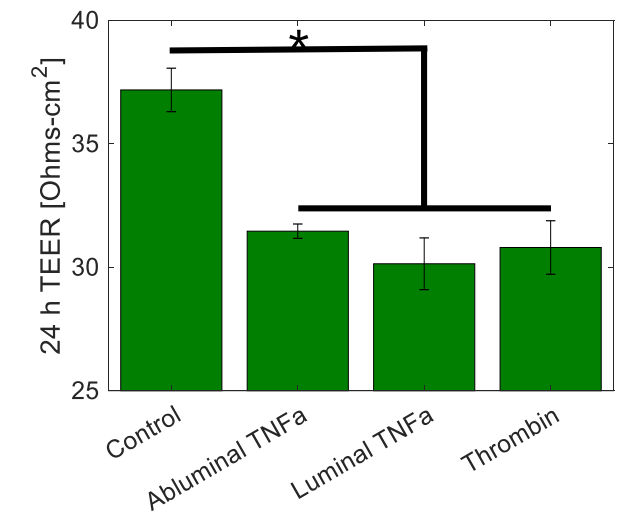


C

VE-Cad
DAPI



D



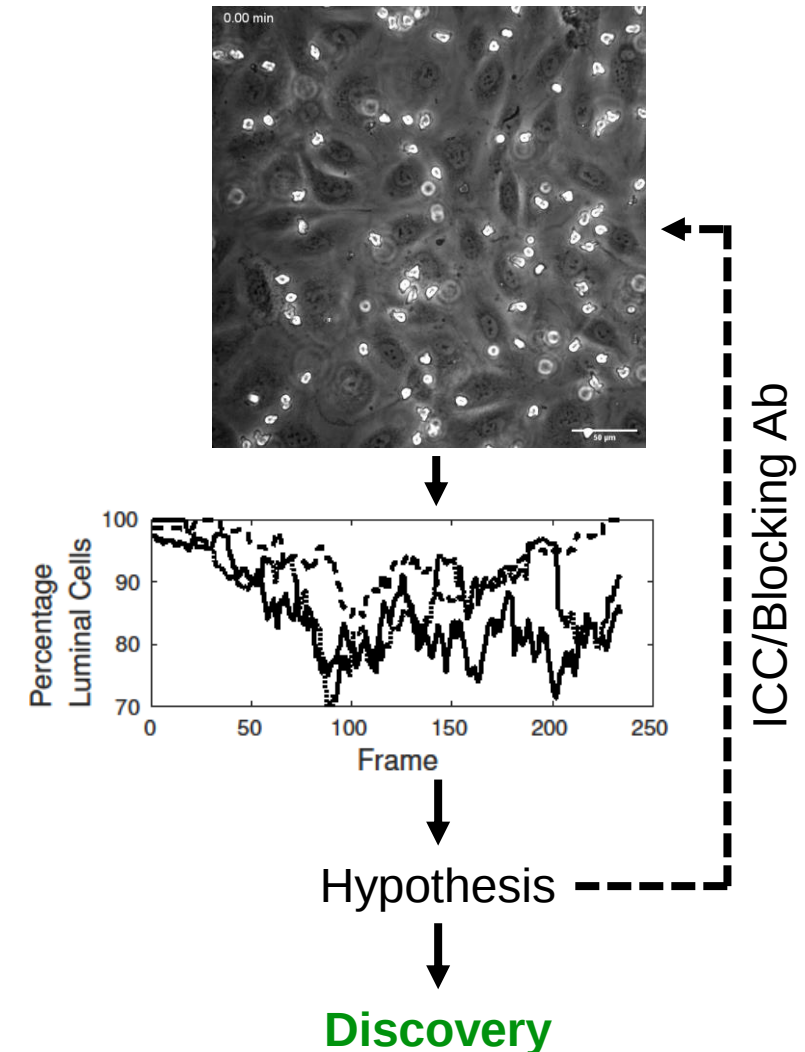
Aim 2 Summary

In Progress

- Improving tracking algorithm
- Head-to-head comparison of automated and hand-tracked data
- Elucidating mechanism of abluminal TNF- α induced PMN transmigration

Future Work

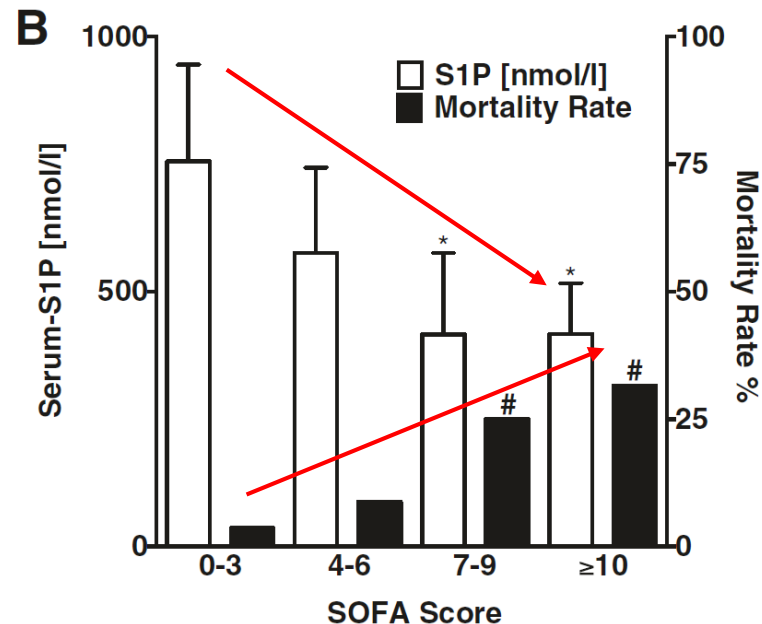
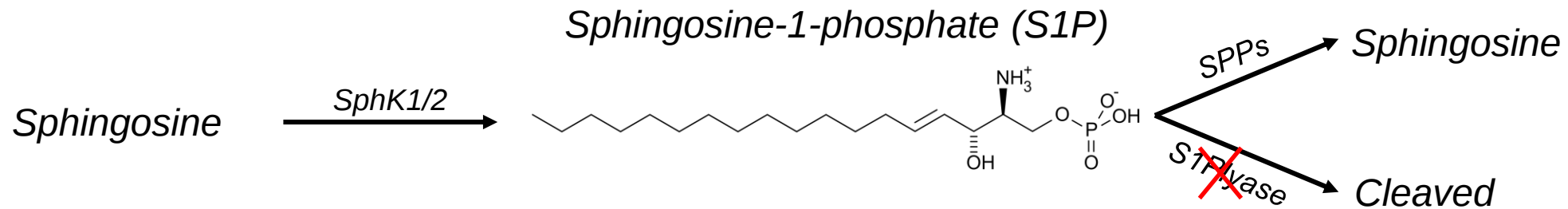
- Utilize primary human pulmonary microvasculature cell lines [PromoCell]
- Investigation endotoxin (LPS) induced immune responses



Specific Aims

1. Develop a facile microvasculature mimetic to quantify small molecule and neutrophil permeability in the presence of physiological shear
2. Elucidate the effects of polarized cytokine and endotoxin delivery on leukocyte dynamics and endothelial cell biology
3. Demonstrate the polarized dependence of S1P in regulating pulmonary vasculature permeability and neutrophil dynamics following septic insult *in vitro*

S1P, Sepsis, and ARDS



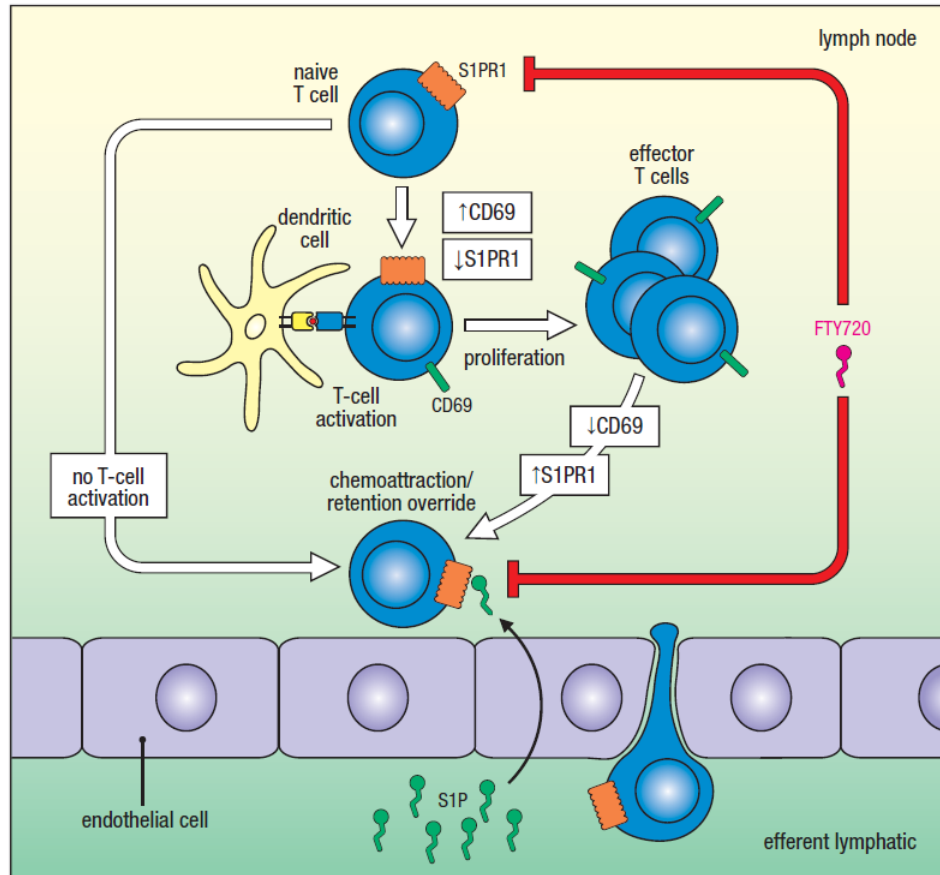
S1P and Sepsis Induced Lung Injury

- S1P is barrier protective in LPS-induced lung injury
- S1PL deficiency protects against LPS-induced acute lung injury

S1P = Sepsis and
ARDS Cure-all

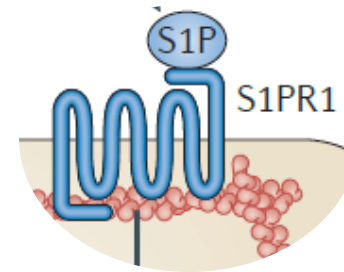


The S1P Paradox

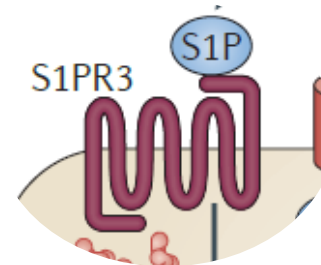


- S1P/S1P₁ regulate lymphocyte egress

S1P signals through 5 GPCRs [S1P₁₋₅]



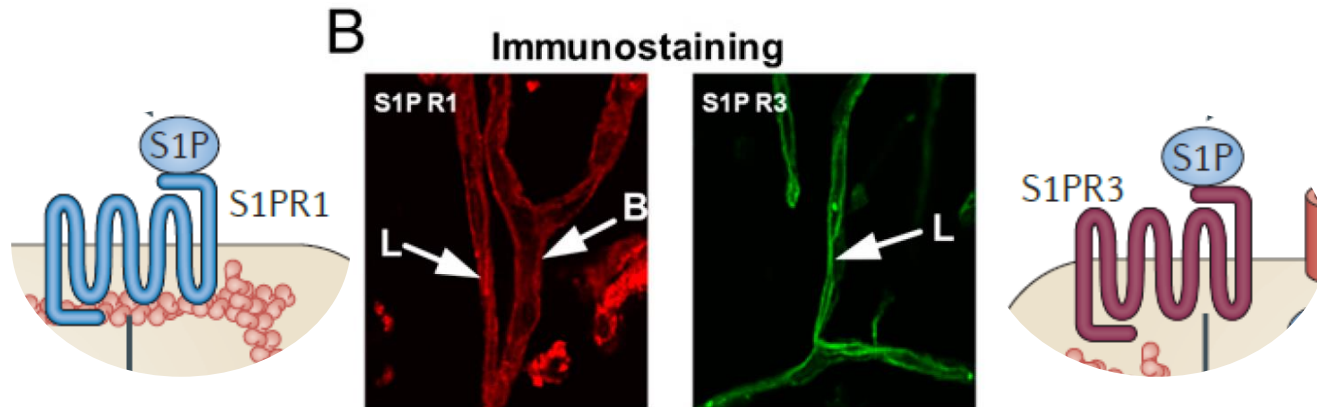
= ↓ EC Permeability



= ↑ EC Permeability,
Leukocyte Recruitment

Natarajan et al., Am J Respir Cell Mol Biol 2013
Nussbaum et al., Nat Commun 2015
Graphic: Spiegel et al., Nat Rev Immunology 2011

EC Apicobasal Polarity and S1P



Cannon et al., PNAS 2012

Guiding Hypothesis: Abluminal delivery of S1P will preferentially target S1P₁ across a broad therapeutic window, without maladaptive immune effects.

Approach

1. Prime the μ SiM-PVB with clinical septic serum
2. Measure leukocyte dynamics and EC permeability in response to serum challenge
3. Demonstrate S1P's polarized ability to alter EC permeability and neutrophil dynamics

Summary

Aim 1: Design and build a facile pulmonary microvasculature barrier mimetic to study EC permeability and PMN dynamics

Aim 2: Elucidate the distinguishing characteristics of the innate immune response to systemic inflammation versus primary infection

Aim 3: Demonstrate the potential of S1P in regulating the innate immune response when delivered abluminally

Acknowledgements

Proposal Exam Committee

Chair: Prof. Danielle Benoit
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 Co-advisor: Prof. Thomas Gaborski
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Timeline

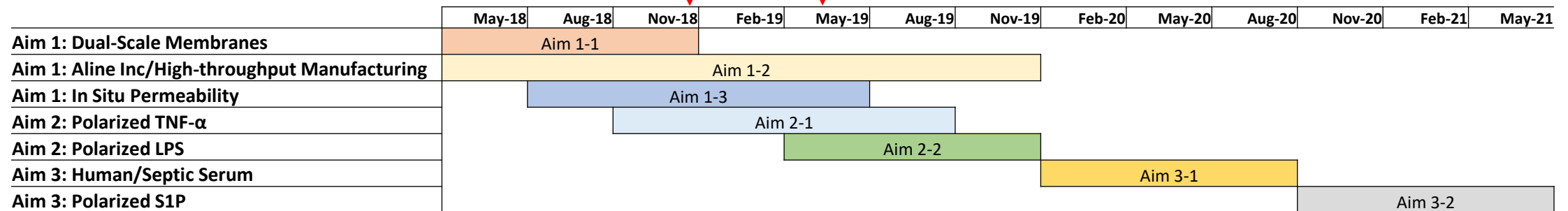
FULL PAPER
Dual-Scale Nanomembranes

Ultrathin Dual-Scale Nano- and Microporous Membranes for Vascular Transmigration Models

Alec T. Salminen, Jingkai Zhang, Gregory R. Madejski, Tejas S. Khire, Richard E. Waugh, James L. McGrath,* and Thomas R. Gaborski*

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An *in vitro* platform for elucidating the molecular genetics of *S. aureus* invasion of the osteocyte lacuno-canalicular network during chronic osteomyelitis



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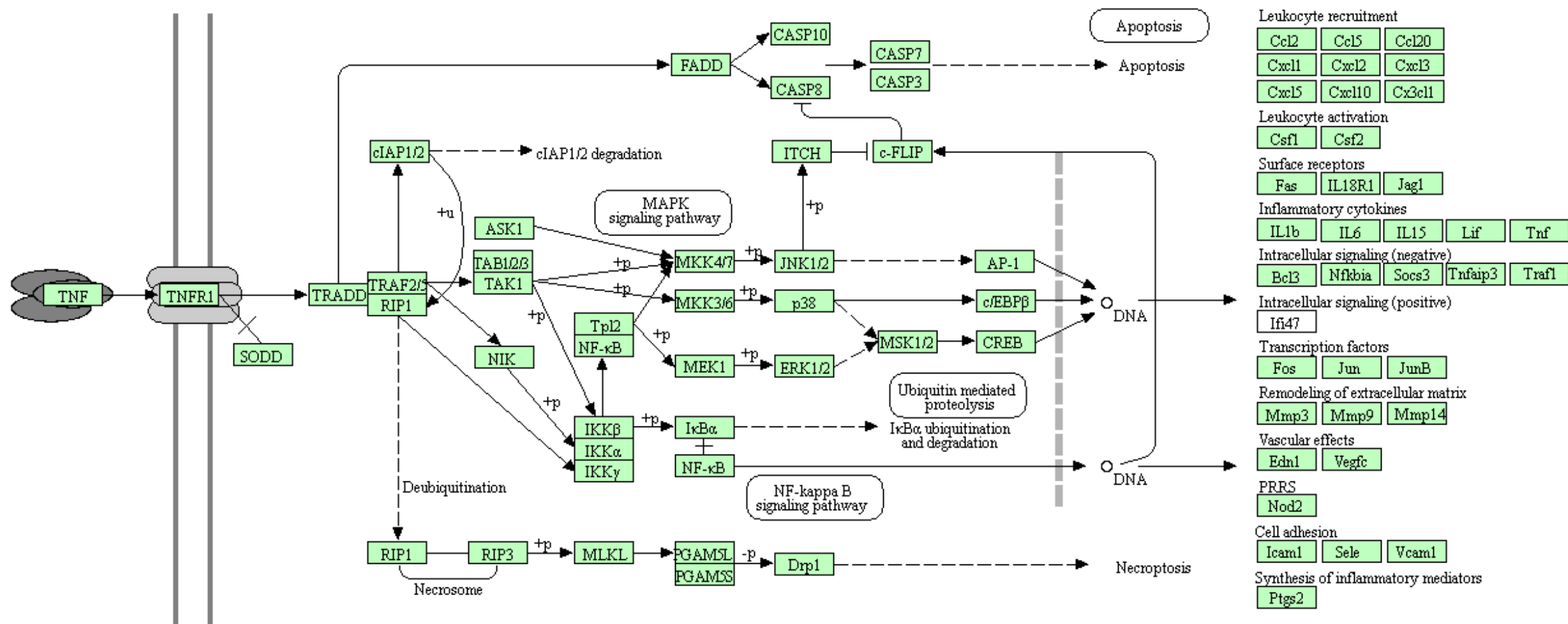
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Supplemental Information

TNF SIGNALING PATHWAY



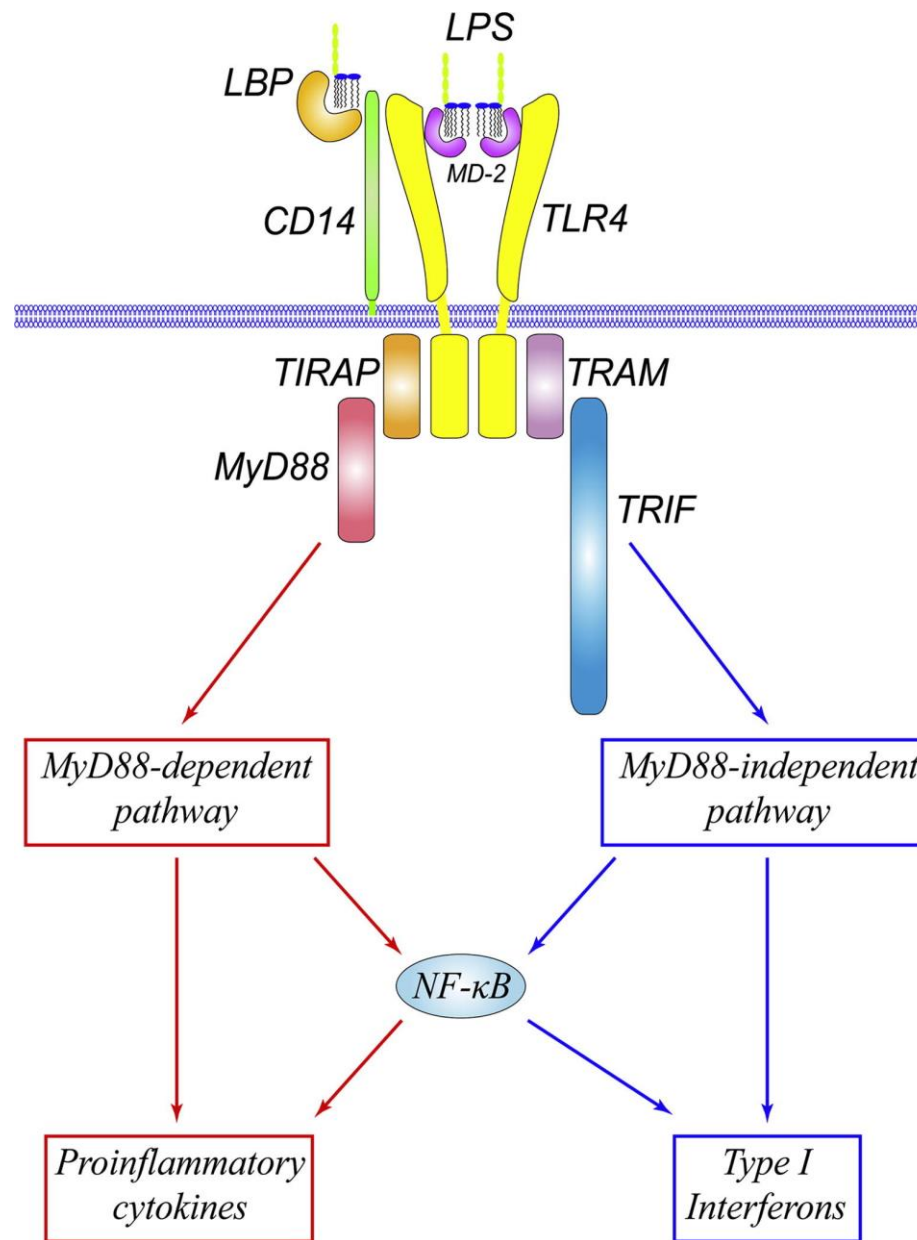


Table 1

The most important neutrophil receptors. See the text for further details.

G-protein-coupled receptors	Fc-receptors	Adhesion receptors	Cytokine receptors	Innate immune receptors
<i>Formyl-peptide receptors</i>	<i>Fcγ-receptors</i>	<i>Selectins and selectin ligands</i>	<i>Type I cytokine receptors</i>	<i>Toll-like receptors</i>
• FPR1 (FPR)	• FcγRI	• L-selectin	• IL-4R	• TLR1
• FPR2 (FPRL1)	• FcγRIIA (human)	• PSGL-1	• IL-6R	• TLR2
• FPR3 (FPRL2)	• FcγRIIB (inhibitory)	<i>Integrins</i>	• IL-12R	• TLR4
<i>Classical chemoattractant receptors</i>	• FcγRIII (mouse)	• LFA-1 ($\alpha_1\beta_2$)	• IL-15R	• TLR5
• BLT1 (LTB ₄ -rec.)	• FcγRIIIB (human)	• Mac-1 ($\alpha_M\beta_2$)	• G-CSFR	• TLR6
• BLT2 (LTB ₄ -rec.)	• FcγRIV (mouse)	• VLA-4 ($\alpha_4\beta_1$)	• GM-CSFR	• TLR7 (?)
• PAFR	<i>Fcα-receptors</i>		<i>Type II cytokine receptors</i>	• TLR8
• C5aR	• FcαRI (human)		• IFNAR (IFNα/β-rec.)	• TLR9
<i>Chemokine receptors</i>	<i>Fcε-receptors</i>		• IFNGR	<i>C-type lectins</i>
• CXCR1 (human)	• FcεRI		• IL-10R	• Dectin-1
• CXCR2	• FcεRII		<i>IL-1R family</i>	• Mincle
• CCR1			• IL-1RI	• MDL-1
• CCR2			• IL1RII (decoy)	• Mcl
			• IL-18R	• CLEC-2
			<i>TNFR family</i>	<i>NOD-like receptors</i>
			• TNFR1 (p55)	• NOD2
			• TNFR2 (p75)	• NLRP3
			• Fas	<i>RIG-like receptors</i>
			• LTβR	• RIG-I
			• RANK	• MDA5
			• TRAIL-R2	
			• TRAIL-R3	

Shear Stress (τ)

$$\rho \left(\frac{\partial v_x}{\partial t} + v_x \frac{\partial v_x}{\partial x} + v_y \frac{\partial v_x}{\partial y} + v_z \frac{\partial v_x}{\partial z} \right) = -\frac{\partial p}{\partial x} + \mu \left[\frac{\partial^2 v_x}{\partial x^2} + \frac{\partial^2 v_x}{\partial y^2} + \frac{\partial^2 v_x}{\partial z^2} \right] + \rho g_x$$

Assumptions: Steady, fully developed, laminar flow, negligible gravity, smooth surfaces, symmetry, parallel plates

$$\frac{\partial p}{\partial x} = \mu \left[\frac{\partial^2 v_x}{\partial y^2} \right]$$

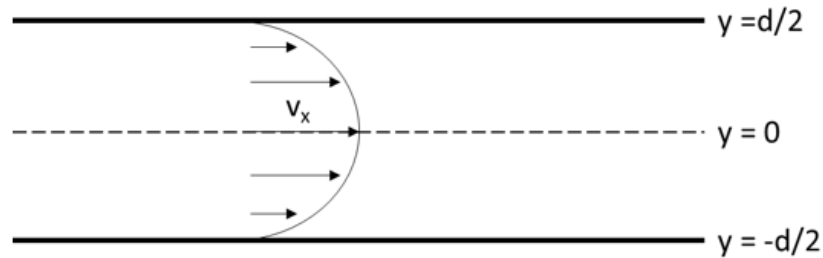
Integrate both sides

$$\frac{\Delta p}{2L} y^2 + C_2 = \mu v_x + C_1 y$$

B.C.

v_x at $y = \mp \frac{d}{2}$ is 0, no slip

$$v_x = \frac{-\Delta p}{2\mu L} \left[y^2 - \left(\frac{d}{2} \right)^2 \right] \longrightarrow \tau = \mu \frac{dv_x}{dy} \longrightarrow \tau_{wall} = \frac{6Q\mu}{d^2 w}$$



μ SiM-PVB

$$\tau = 4.5 \text{ dyn/cm}^2$$

$$\mu = 8.9 \times 10^{-3} \text{ dyn. s/cm}^2$$

$$d = 0.043 \text{ cm}$$

$$w = 0.2 \text{ cm}$$

$$Q = 1.87 \text{ mL/min}$$

Entrance Length (L)

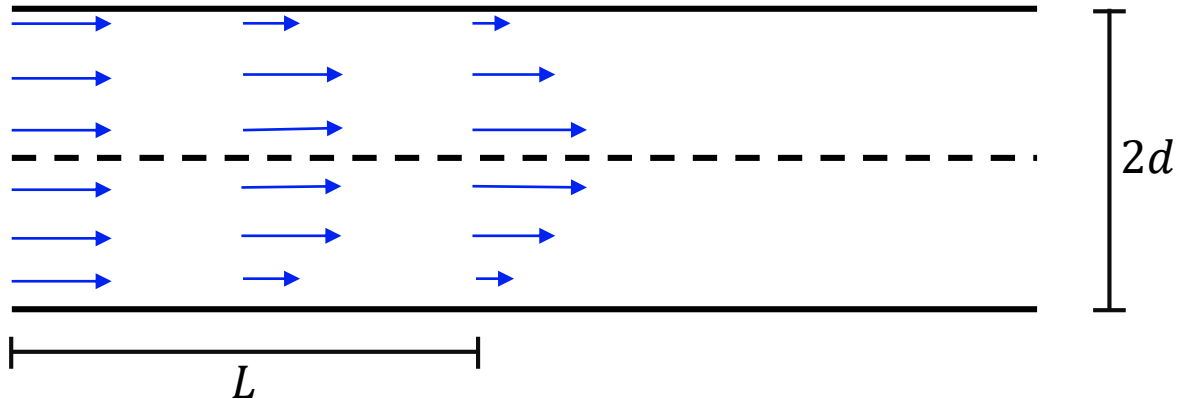
$$L = 0.1048 \frac{\rho u d^2}{\mu}$$

ρ = density of the fluid

μ = viscosity of the fluid

d = half plate separation

u = velocity of the fluid



μ SiM-PVB

$$\rho = 997 \text{ kg/m}^3$$

$$\mu = 8.9 \times 10^{-4} \text{ Pa} \cdot \text{s}$$

$$d = 0.0215 \text{ cm}$$

$$V = 0.036 \text{ m/s}$$

$$L = 0.195 \text{ mm}$$

Reynolds number (Re): μ SiM-PVB

$$Re = \frac{\text{inertial forces}}{\text{viscous forces}} = \frac{\rho u^2}{(\mu u/D)} = \frac{\rho u D}{\mu}$$

ρ = density of the fluid

μ = viscosity of the fluid

D = diameter of the channel

u = velocity of the fluid

$$\text{Hydraulic mean diameter } (D_e) = \frac{4A}{P}$$

A = cross-sectional area

P = wetted perimeter

μ SiM-PVB

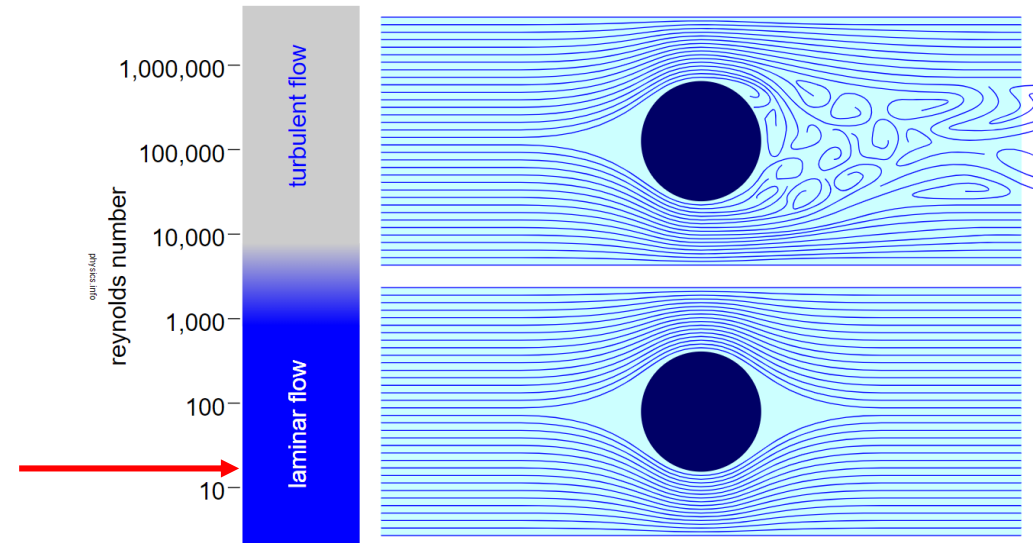
$$\rho = 997 \text{ kg/m}^3$$

$$\mu = 8.9 \times 10^{-4} \text{ Pa} \cdot \text{s}$$

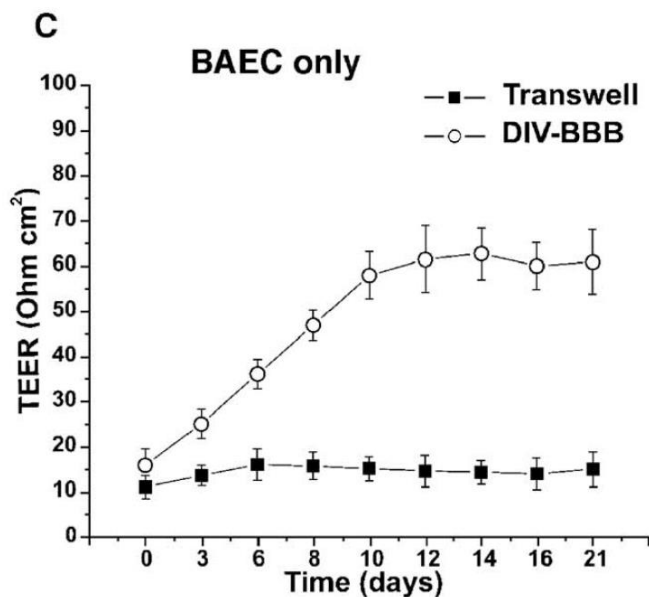
$$D_e = 7.08 \times 10^{-4} \text{ m}$$

$$u = 0.036 \text{ m/s}$$

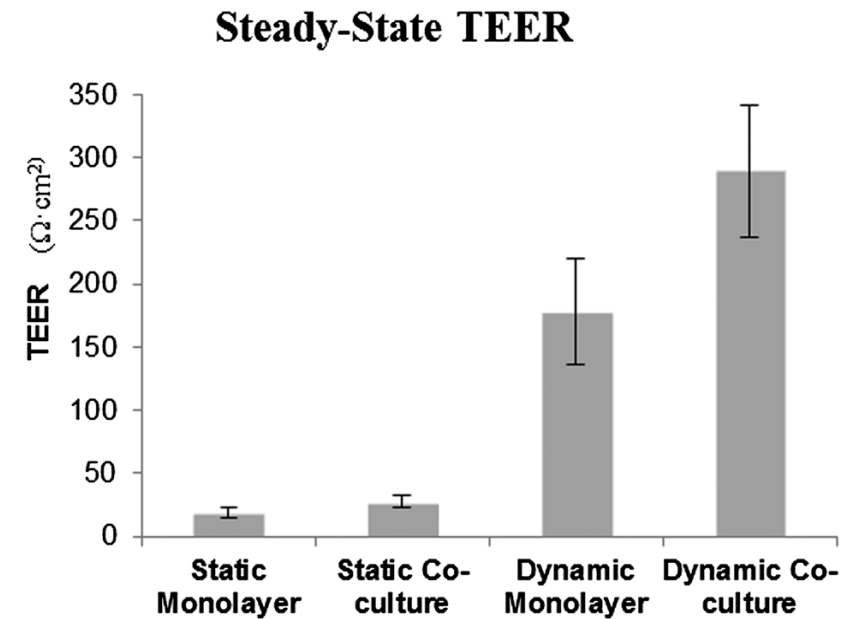
$$\underline{Re \sim 29}$$



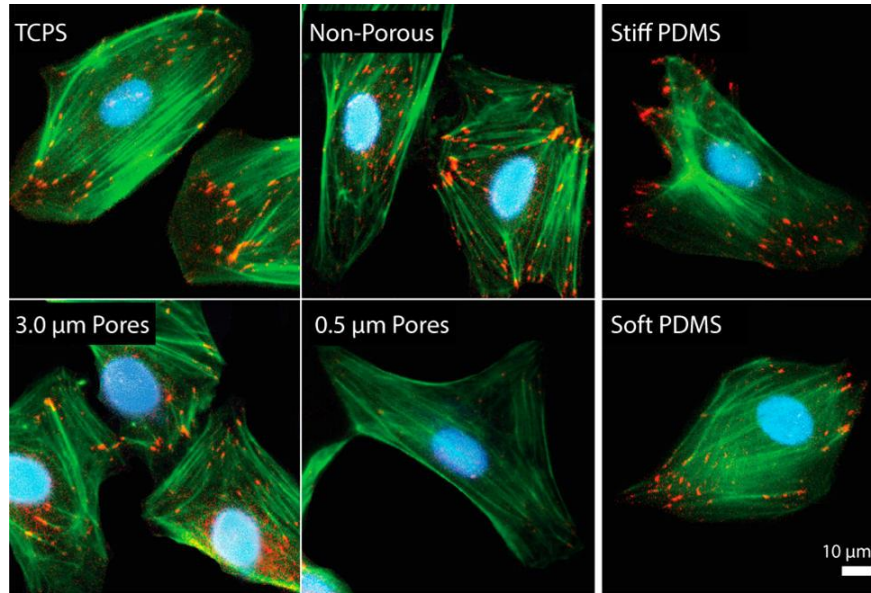
Shear Stress Improves EC Barrier *In Vitro*



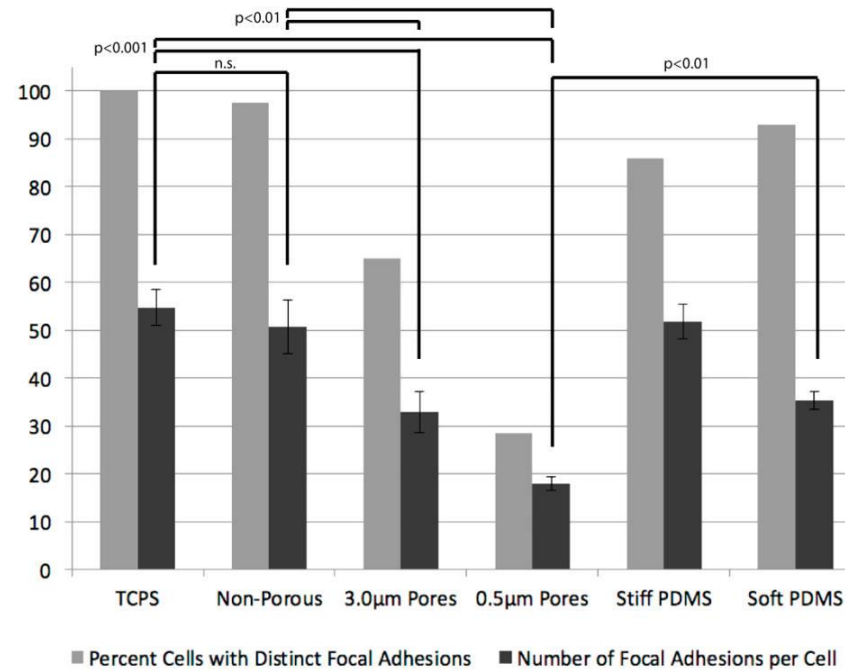
Santaguida et al., Brain Res. 2006

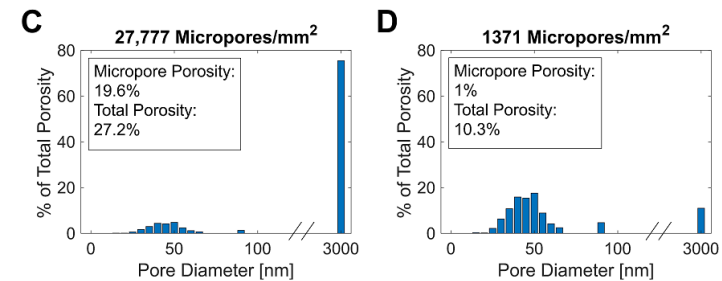
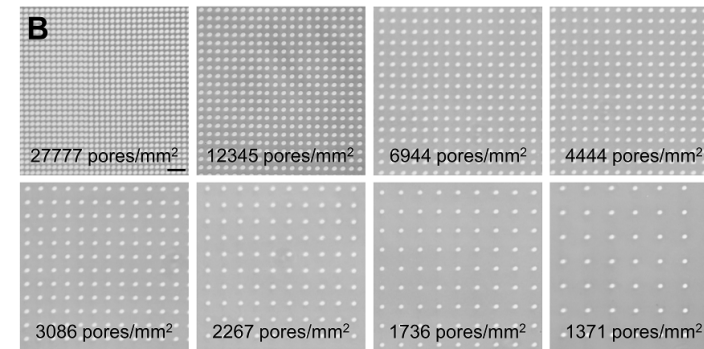
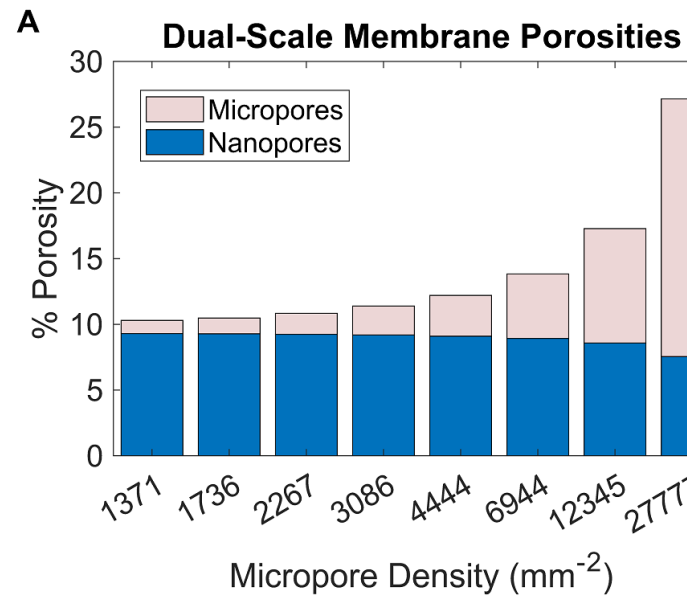
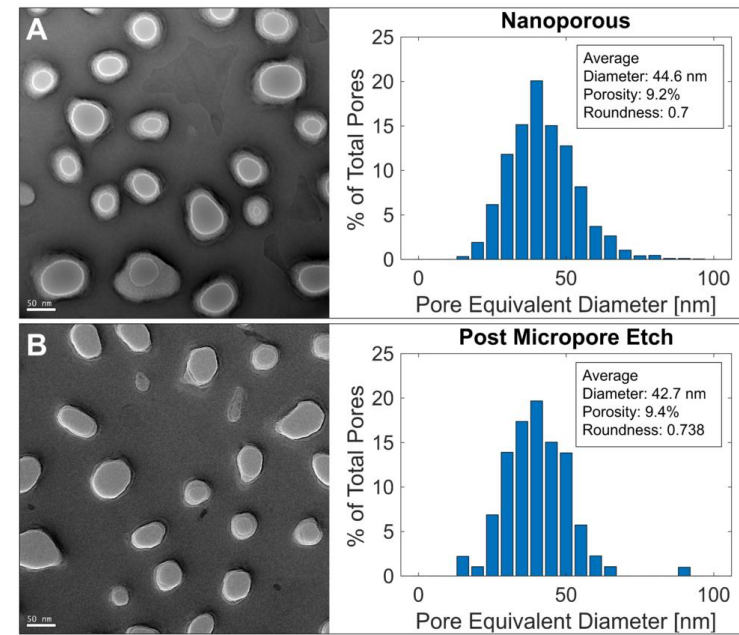
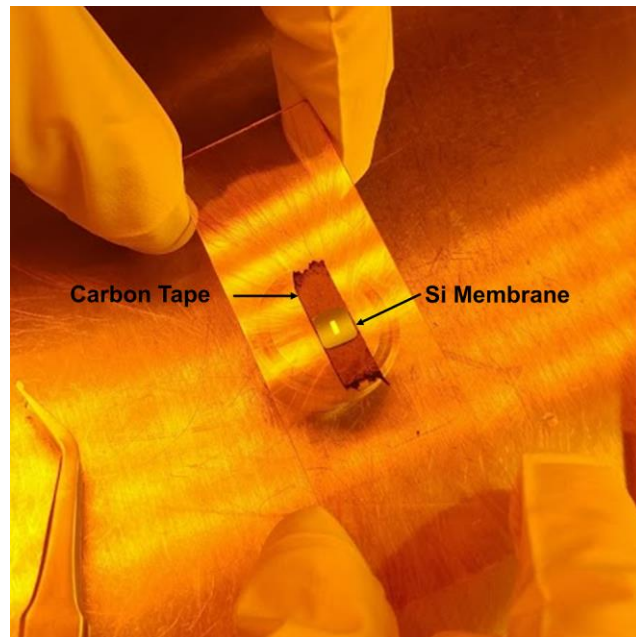


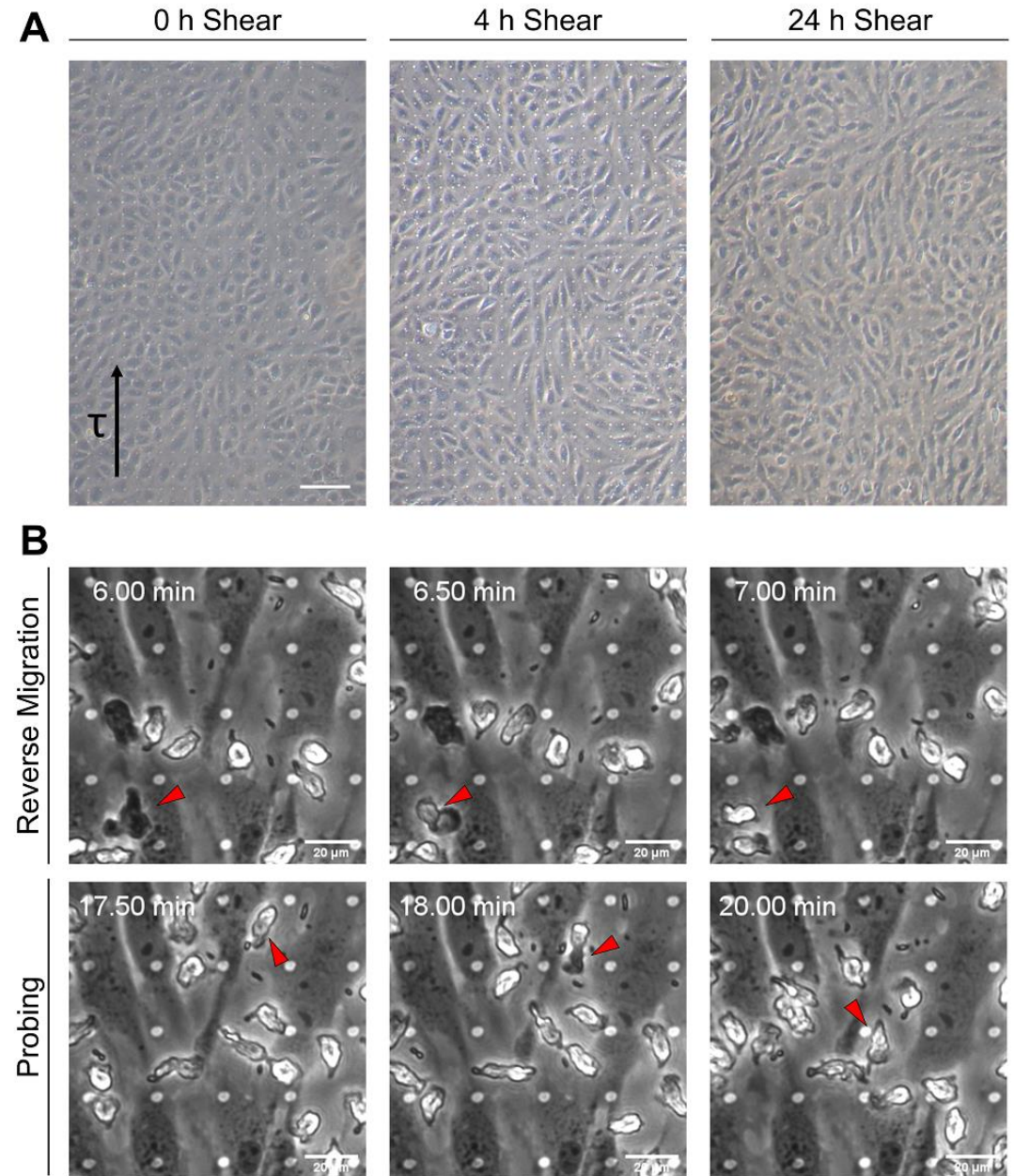
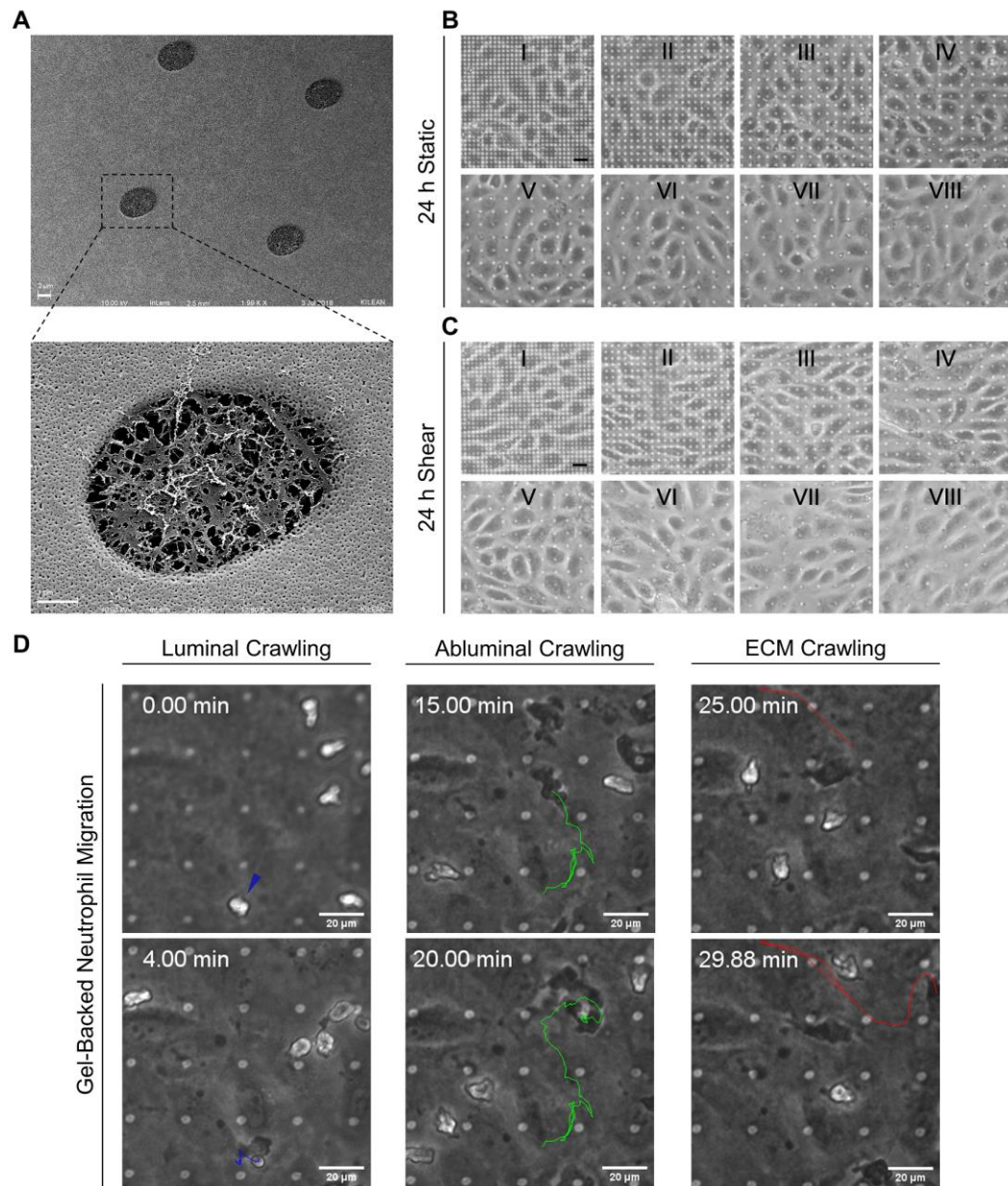
Booth et al., Lab Chip 2006



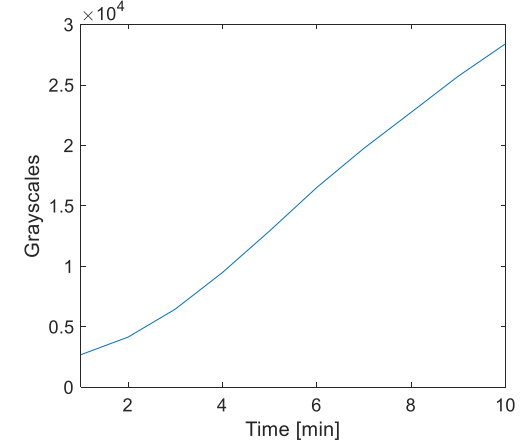
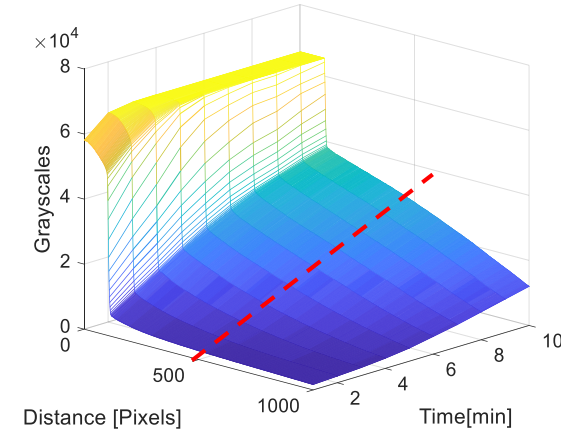
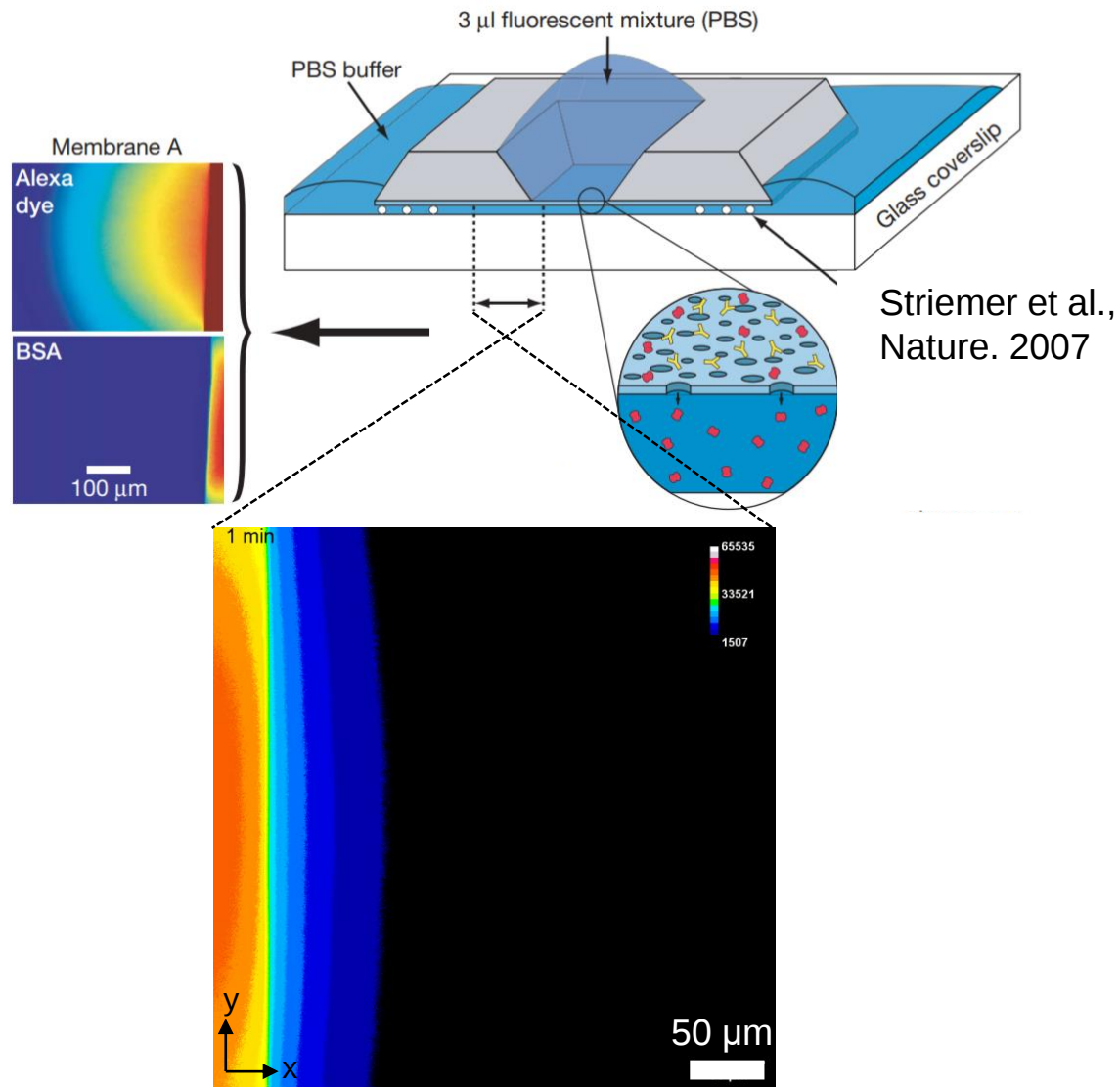
Casillo et al., ACS Biomater. Sci. Eng. 2017







In Situ Permeability Measurements



Question: How do Fick's laws of diffusion govern concentration change through a point over time?

$$C_x = C_o \operatorname{erfc} \left(\frac{x}{2\sqrt{Dt}} \right) \quad \propto \quad I_x = I_o \operatorname{erfc} \left(\frac{x}{2\sqrt{Dt}} \right)$$

Crank., The Mathematics of Diffusion

Diffusion Function Derivation

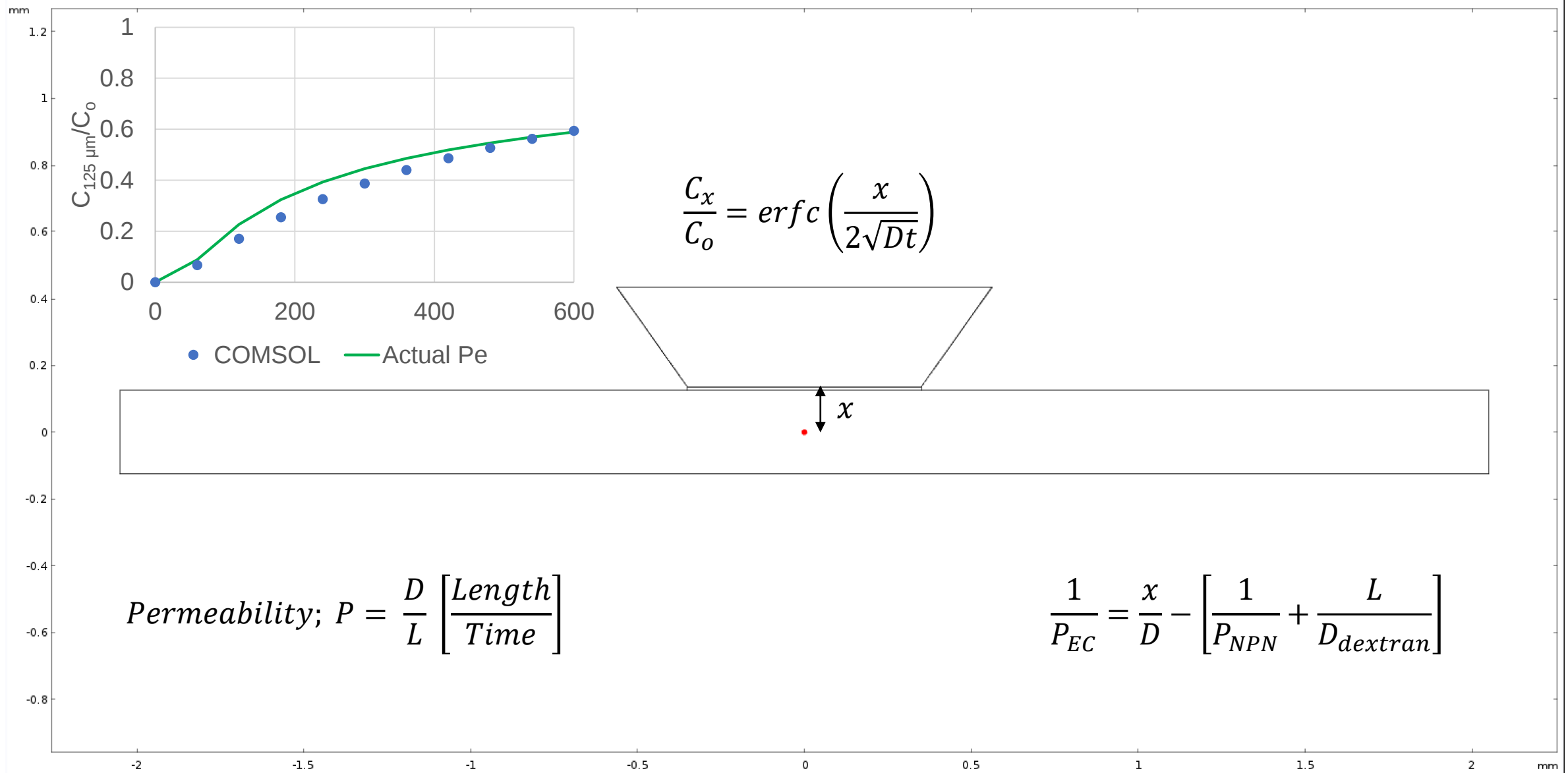
Solution of Fick's Second Law in Semi-Infinite Medium with a Constant Source

$$\frac{\partial C}{\partial t} = D \frac{\partial^2 C}{\partial x^2}$$

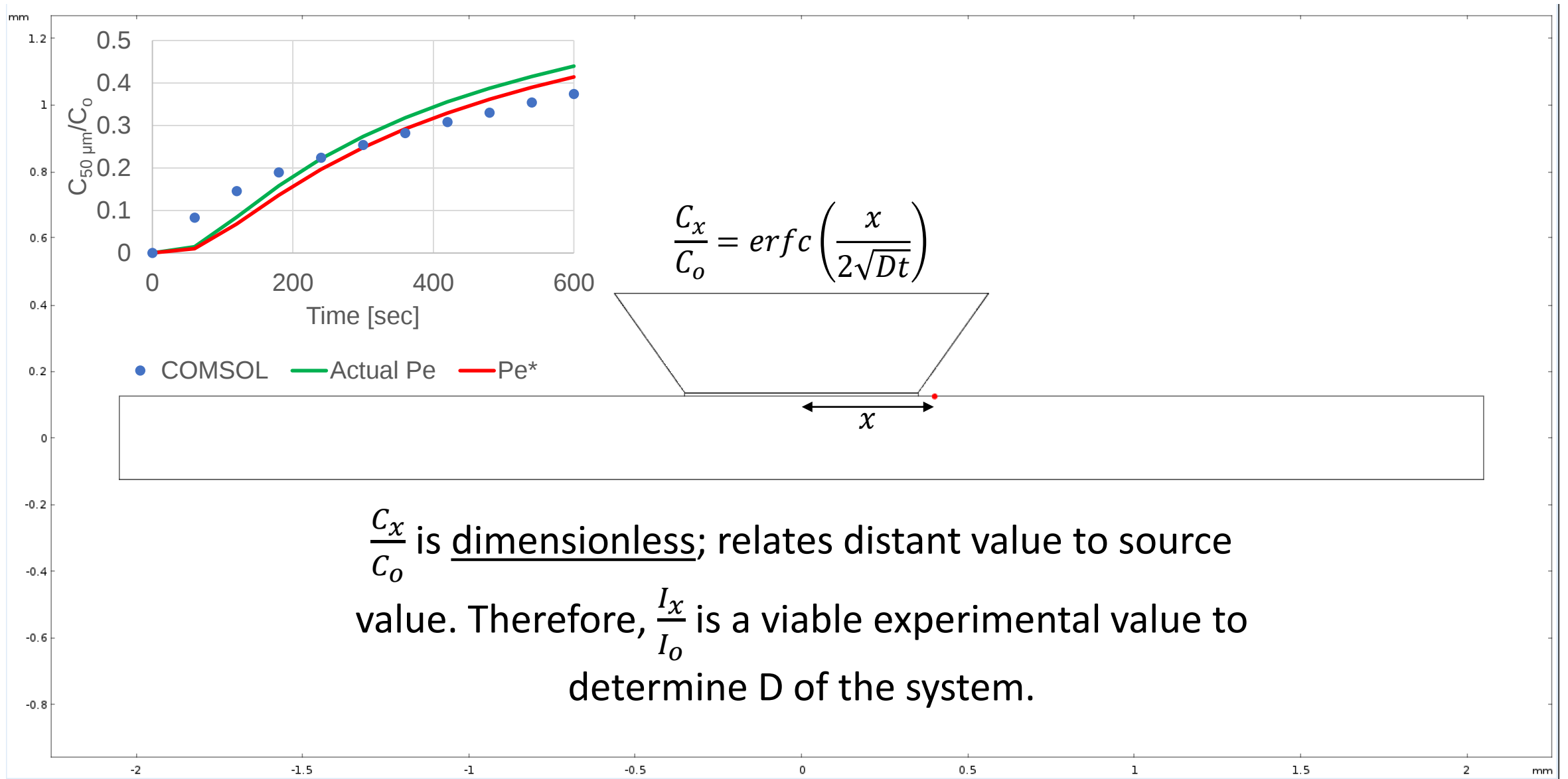
B.C. $C = C_o, x = 0, t > 0$
 $C = 0, x > 0, t = 0$

$$C_x = C_o \operatorname{erfc} \left(\frac{x}{2\sqrt{Dt}} \right) \quad \propto \quad I_x = I_o \operatorname{erfc} \left(\frac{x}{2\sqrt{Dt}} \right)$$

Ideal COMSOL Configuration



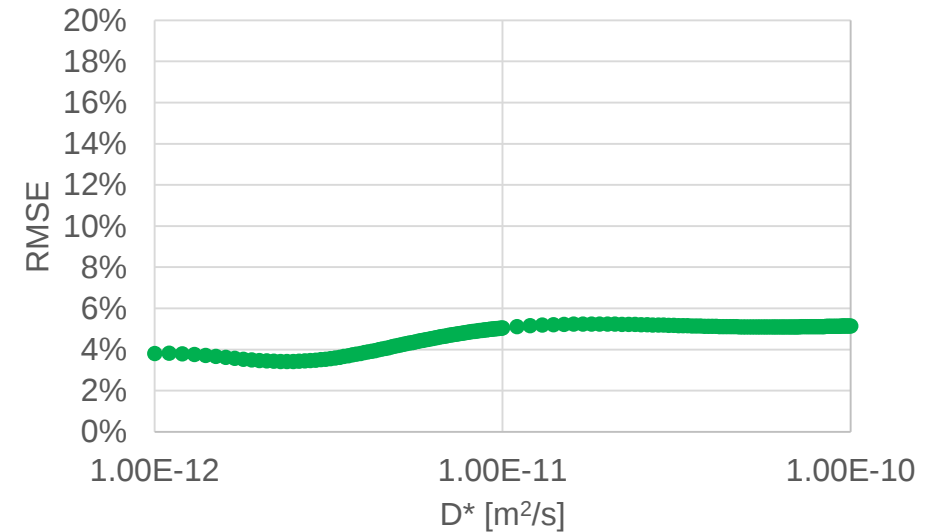
Experimental COMSOL Configuration



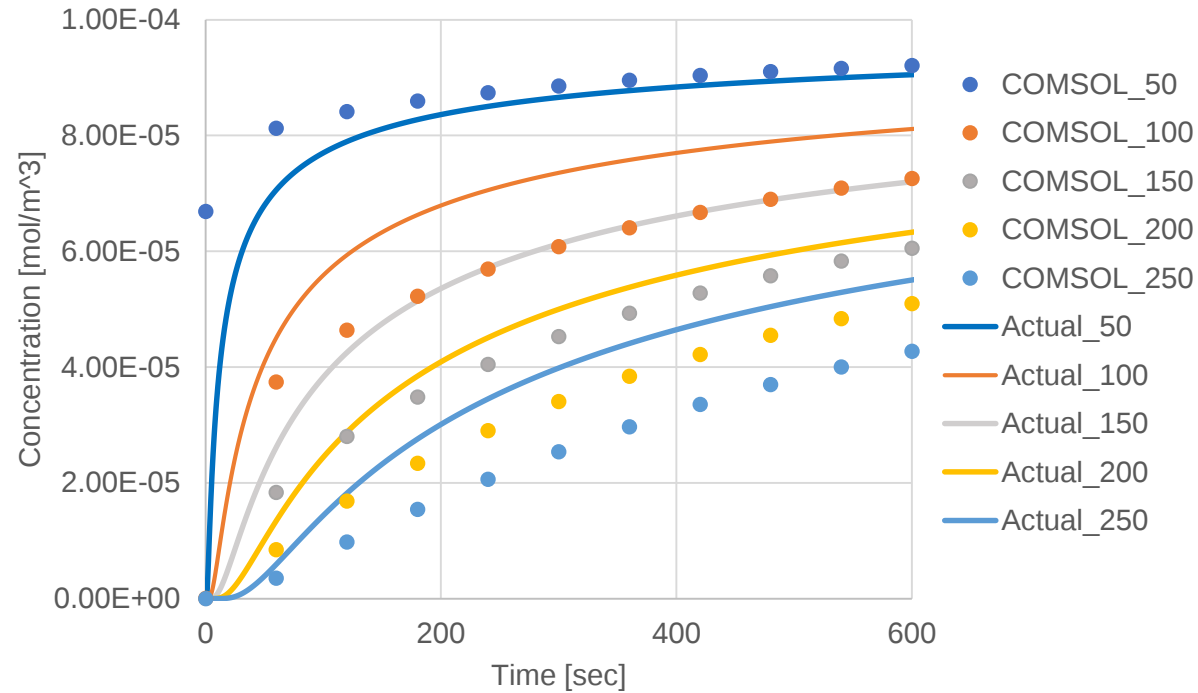
RMSE: COMSOL vs Analytical

Validating Our Model

- Parametric sweep of 200 'Pe' values
- RMSE compares COMSOL data for concentration to analytical data
- RMSE is consistent around 5%
- Lowest RMSE through iterative check was comparable

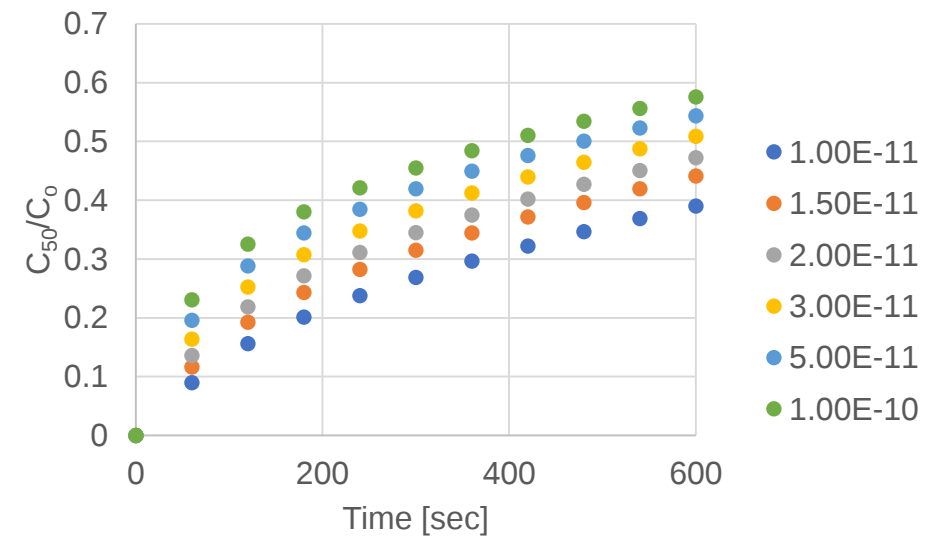
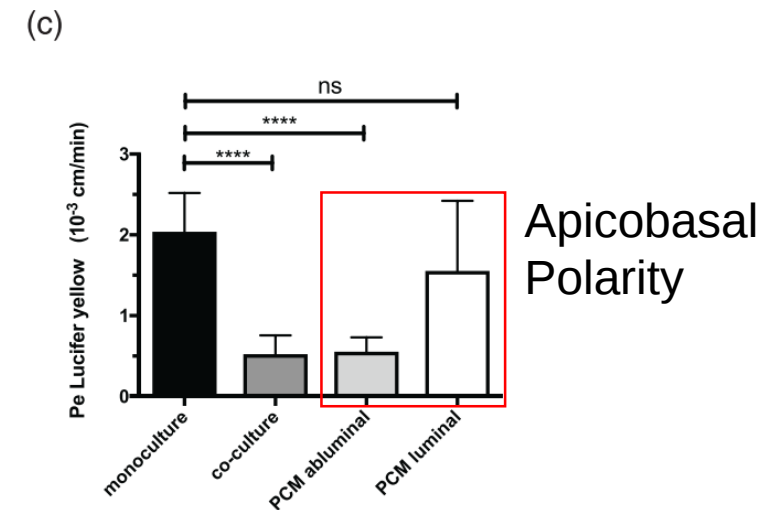
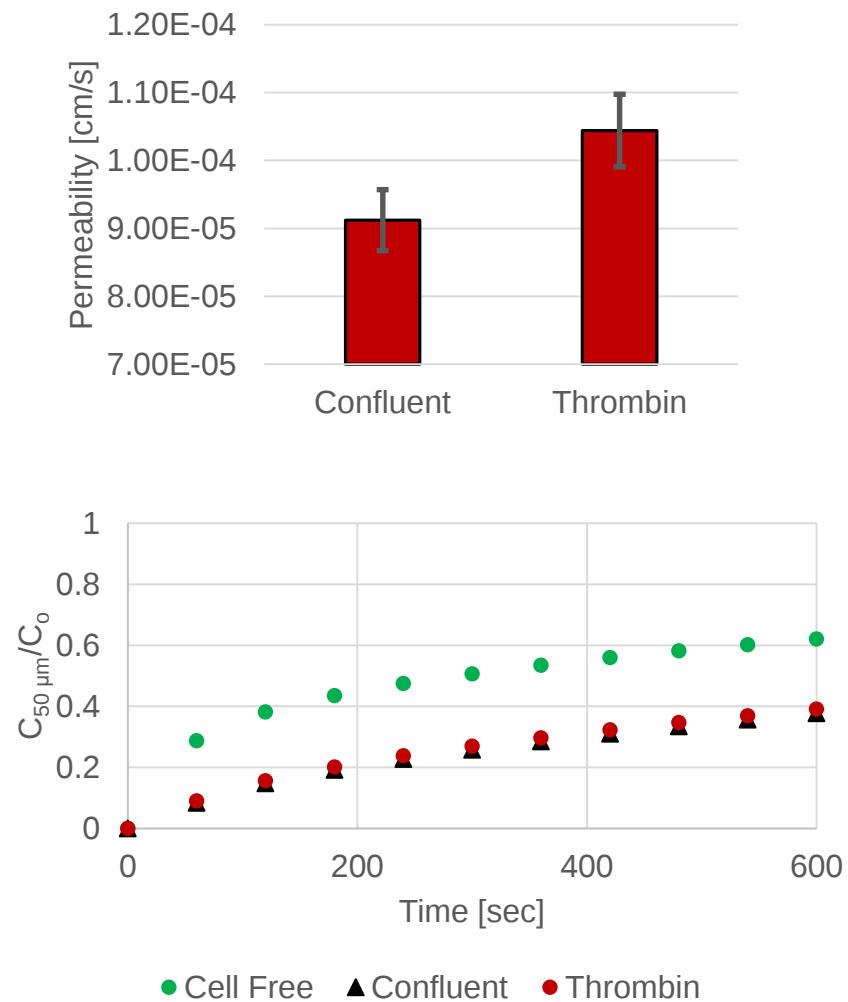


Solution Falls Apart as x Increases

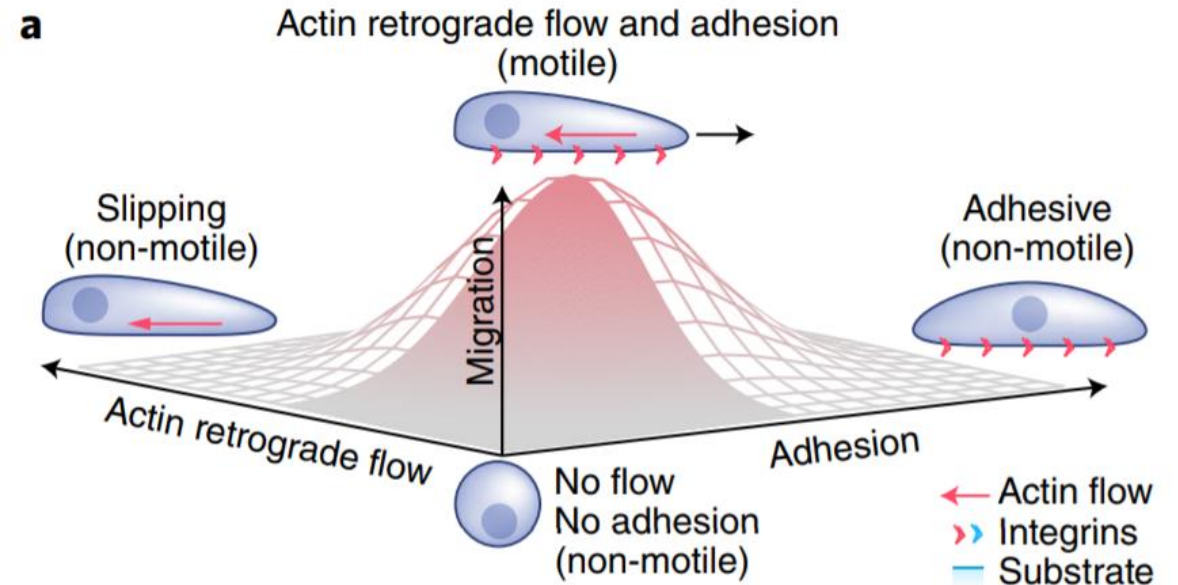
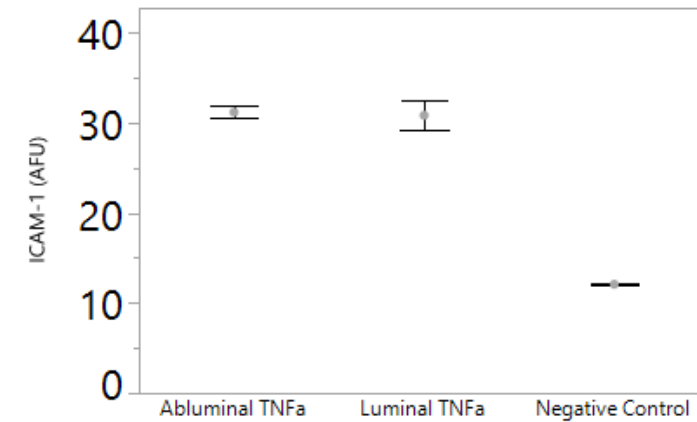
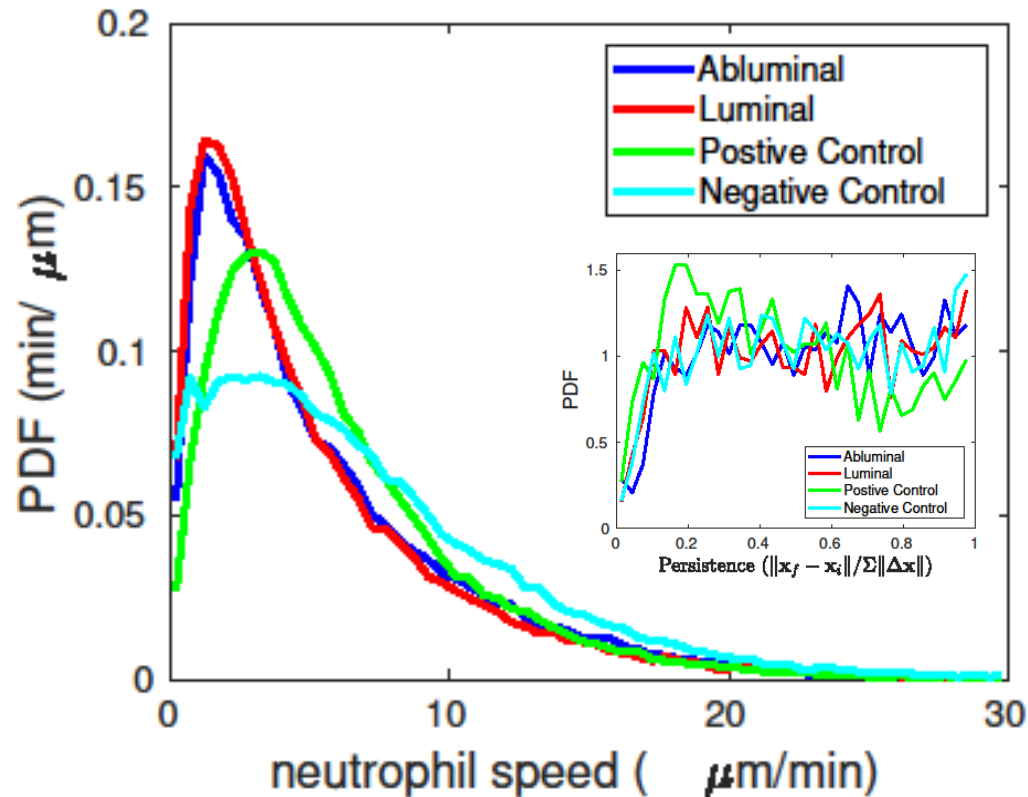


$\uparrow x = \uparrow \text{Root Mean Square Error}$

Transwell Data



Increased ICAM-1 Decreases PMN Velocity

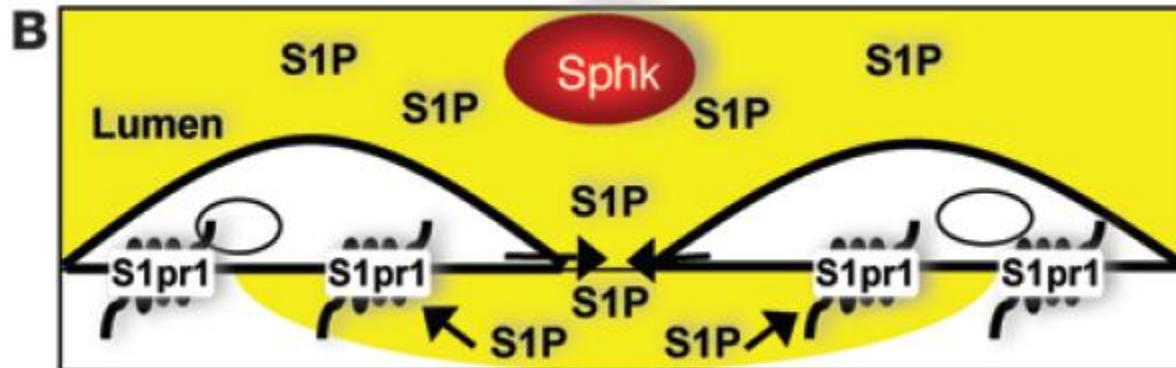


Sphingosine-1-phosphate in the plasma compartment regulates basal and inflammation-induced vascular leak in mice

Eric Camerer,^{1,2,3} Jean B. Regard,¹ Ivo Cornelissen,¹ Yoga Srinivasan,¹ Daniel N. Duong,¹ Daniel Palmer,¹ Trung H. Pham,⁴ Jinny S. Wong,⁵ Rajita Pappu,¹ and Shaun R. Coughlin^{1,2}

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⁵Gladstone Institutes, San Francisco, California, USA.



Level of receptor versus downstream effectors?